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Computer Vision for Ambient Assisted Living Monitoring Systems for Personalized Heal and Wellness That Are Robust in the Real V and Accepted by Users, Carers, and Societ	thcare World Sy
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Abstract	
The Amhient Assisted Living (AAL) paradiam proposes advanced tech	nologies and
services to improve the quality of life health and wellbeing of citizer	ns hy making
their daily-life activities easier and more secure by monitoring patients	under snecifi
treatment and by addressing at-risk subjects with proper courseling. T	he challenge
brought by AAL range from robust accurate and nonintrusive data acqui	isition in daily

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1	users and that support long-term engagement. This chapter offers a brief survey of ex-	1
2	isting vision-based monitoring solutions for personalized healthcare and wellness, and	2
3	introduces the Wize Mirror, a multisensory platform featuring advanced algorithms for	3
4	cardiometabolic risk prevention and quality-of-life improvement.	4
5	Keywords	5
6		6
7	Amplent assisted living (AAL), self-monitoring, Unobtrusiveness, user engagement, Physiological monitoring Wellness index	7
8	Thysiological monitoring, weintess mack	8
9		9
10	6.1 INTRODUCTION	10
11	The term Ambient Assisted Living (AAL) concerns ICT ¹ solutions embed-	11
12	ded in the living environment to monitor the setting and the behavior of its	12
13	occupants in real time. AAL solutions can go beyond observing; they can	13
14	move towards interacting by communicating with the user via prompts,	14
15	triggering assistance from emergency services, and providing up-to-date	15
16	information to families and caregivers.	16
17	AAL technologies trace their roots back to home automation and as-	17
18	sistive domotics; they are now applied in many different scenarios, from	18
19	telecare to pervasive wellness [1,2]. The main aim is improving the quality	19
20	of life, health, and wellbeing of citizens; making their daily-life activities	20
21	easier and more secure; monitoring and curing ill or at-risk subjects; and	21
22	even performing primary prevention in healthy subjects.	22
23	The three main targets of AAL solutions are	23
24	• monitoring (and acting on) environmental conditions (e.g. lights, tem-	24
25	perature, opening of doors, gas detection) for the occupants' safety and	25
26	comfort;	26
27	• monitoring human activity and behavior, from basic motion tracking	27
28	and human activity recognition up to long-term behavioral analysis;	28
29	• monitoring human physiological signs (physical, clinical, vital, emo-	29
30	tional parameters) for personalized healthcare and wellness, including	30
31	telerehabilitation, cure management, and prevention.	31
32	The general scheme of AAL solutions is to enrich the environment with	32
33	a distributed sensor system. The sensors include ambient sensors (e.g. mag-	33
34	netic switches, photosensors) as well as body or wearable sensors that are fixed	34
35	to the human body or clothing (e.g. gyroscopes, pulse oximeters). A large	35
36	network of sensors are often needed to gather enough data to accomplish	36
3/ 28	the complex tasks required for AAL applications; therefore, systems may be	37
38 20		36
39	 Information and Communication Technology. 	35

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costly to maintain, highly sensitive to a sensor's performance, and obtru-sive. Obtrusiveness is an issue especially for wearable sensors, due to their weight, effects on the skin, and burden on the subject during daily-life activities. Recently, video cameras (including standard and depth cameras) and computer vision techniques came into the spotlight as alternative so-lutions for AAL applications [3,4]. Video-based AAL solutions benefit from the maturity of the research in computer vision: decades of stud-ies, boosted by needs in domains such as security and surveillance, have brought robust techniques for interpreting the rich information provided by cameras. Also, video-based solutions can favor the acceptability of AAL systems: video cameras are expected to reduce the possible anxi-ety towards new technologies, even for the elderly, as they are familiar objects. Moreover, cameras may be perceived as less invasive than other sensors as they do not require any physical contact with the subject, they do not have to be worn (with the exception of wearable cameras), and they can be fitted in the home setting by taking aesthetics into ac-count. Another main advantage of video and depth cameras is that they can register a great deal of information compared to other sensors, and al-low the analysis of complex scenarios. A single camera can capture most of the activities performed in a room; therefore, in principle, it could replace many sensors. This would cut costs, also thanks to the fact that high-quality cameras are now available at affordable prices. Moreover, the same hardware setup can serve for multiple applications by just changing the software analyzing the visual data. Therefore, computer vision supports flexible and adaptive solutions, which can be easily extended and updated on demand. 6.1.1 Chapter Scope There is a huge corpus of work on the use of computer vision for ambient monitoring and navigation and for activity recognition [5]. These topics are also covered in other chapters of this book. Therefore, after a brief introduction to the field of computer vision for AAL (Section 6.2), this chapter focuses on the use of computer vision techniques for monitoring human physiological signs in AAL solutions for personalized healthcare and wellness. In Section 6.3, we discuss the monitoring through videos, images, and 3D data, of • vital signs (heart rate and respiratory rate);

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1	• posture and movement, especially for rehabilitation;	1
2	• morphological parameters (e.g. body mass index);	2
3	• emotional state (e.g. stress and anxiety).	3
4	Subsequently, in Section 6.4, we identify barriers and challenges for	4
5	vision-based AAL solutions to reach their full maturity and applicability,	5
6	especially within the healthcare domain.	6
7	Finally, as a possible solution, we introduce the Wize Mirror, a multisen-	7
8	sory platform for health and wellbeing monitoring (Section 6.5). The Wize	8
9	Mirror features advanced computer vision algorithms for cardiometabolic	9
10	risk assessment through facial analysis.	10
11	Our target audience includes researchers and healthcare professionals,	11
12	who will find information about the aspects that may affect their practice.	12
13		13
14		14
15	0.2 CONFORER VISION FOR AAL	15
16	The traditional three-step pipeline for video-based AAL solutions includes	16
17	image/video acquisition, preprocessing (segmentation of the region of in-	17
18	terest, filtering for noise reduction, or contrast enhancement), and feature	18
19	extraction and interpretation. The acquisition devices include traditional	19
20	RGB cameras (including omnidirectional cameras and wearable cameras	20
21	for egocentric vision); thermal cameras that acquire the infrared radiation	21
22	of the scene; MultiSpectral Imaging (MSI) systems [6]; and depth sensors,	22
23	based either on time of flight or on structured light [7]. Depth sensors in	23
24	particular have became very popular lately because of their decreasing cost	24
25	and the advantages they provide, including robustness to changing lighting	25
26	conditions and protection of privacy since the appearance of a person is not	26
27	recognized in depth images.	27
28	The architecture of a video-based AAL solution traditionally consists of	28
29	a set of cameras for data capture connected to a server; processing modules	29
30	for data processing and analysis; and an alert/decision module, which may	30
31	or may not include a human operator. This solution can ease the integra-	31
32	tion of data from different sources, but usually requires high bandwidth	32
33	for data transmission, unless compressed video is used for transmission.	33
34	An alternative band-saving solution is given by distributed smart camera	34
35	networks that analyze the data locally and only transmit the alert/deci-	35
36	sion [8].	36
37	One of the main challenges of video-based AAL systems is the robust-	37
38	ness with respect to the operating conditions in real-life settings. A first	38
39	issue for robust data acquisition is what cameras are able to see, which	39

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depends on the viewing angle and user positioning with respect to the camera, but also on occlusions and clutter. The problem of the viewing an-gle of the scene can be solved via hardware or software solutions. A solution often adopted in ambient surveillance systems is based on omnidirectional cameras which can capture virtually a 360 degree viewing angle of data. Al-ternatively, view-invariant computer vision algorithms are required, based either on single cameras or on image fusion strategies from multiple cam-eras. Multiple cameras and image fusion strategies may also help to solve the problem of occlusions that are likely to occur in a room. Finally, face recognition and the ability to track (multiple) people are needed in case of multiple occupants of the monitored space. Another major concern for video-based assistive technologies is pri-vacy. AAL systems imply the collection of information in private spaces about individual subjects and their lives. With image and video record-ings, the privacy protection issue becomes even more prominent since the occupants' identities are shown. Privacy protection is considered urgent es-pecially if image data are stored and transmitted to a server, and if they are expected to be analyzed by designated carers. The consequences can be low acceptance by the end users, and even techniques for avoiding the camera to sabotage the monitoring [9]. Striking a happy medium between the benefits of image and video recording and the potential privacy loss requires focusing on the perspective of the end user. Some studies [10,11] have suggested that people would be willing to accept video-based activ-ity monitoring systems, in principle, if they felt that the technology would make a real difference to their lives, and if they were really in need of assistance. Also, improving the reliability of systems so that they do not require images to be analyzed by humans could improve confidentiality. Again, a possible solution is given by smart cameras, which can perform a part of the image and video processing locally, and either only transmit decision information to carers or filter the data to obscure individual iden-tities [8]. 6.3 MONITORING IN PERSONALIZED HEALTHCARE AND WELLNESS: THE STATE OF THE ART

The home can be a focal point for ensuring healthy living if it is equipped with the right infrastructure: AAL systems based on computer vision solutions can support health status monitoring for the management of chronic diseases and rehabilitation therapies, but also for the prevention of disease

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1	and improvement of individual wellbeing through the achievement and	1
2	maintenance of a healthy lifestyle. These systems may become part of the	2
3	medical toolbox for healthcare professionals, who could benefit from inno-	3
4	vative communication and monitoring facilities.	4
5	The parameters to be monitored include vital signs such as heart rate and	5
6	respiratory rate (Section 6.3.1); measures related to posture and movement,	6
7	especially during rehabilitation (Section 6.3.2); morphological parameters	7
8	of the body and face related to risk factors such as overweight and obesity	8
9	(Section 6.3.3); and descriptors of the affective state, such as cues about the	9
10	onset and progression of different diseases (Section 6.3.4).	10
11		11
12	6.3.1 Vital Signs	12
13	The monitoring of vital signs includes the estimation of	13
14	• heart rate (HR);	14
15	• heart rate variability (HRV);	15
16	• respiratory rate (RR).	16
17		17
18	Heart Rate	18
19	Heart rate monitoring is important by virtue of the significance of this vital	19
20	sign in both health and disease. Physiological changes in HR can be as-	20
21	sessed during exercise or during sleep when a reduction in HR may occur	21
22	due to prevalence of vagal drive. In disease, there is an association between	22
23	HR and outcome in heart failure patients, and a baseline HR is considered	23
24	a cardiovascular risk factor. A special application of HR monitoring can	24
25	be reported in the aging population as HR can also be a sign of improper	25
26	movements. Since an increasing number of older subjects wish to live in	26
27	their home environments rather than moving into care facilities, the op-	27
28	portunity to unobtrusively monitor HR is challenging. Therefore, several	28
29	studies have been performed to evaluate whether the HR can be assessed	29
30	from video streams [12], thus avoiding the use of wearable sensors.	30
31	A commonly adopted approach to HR assessment is based on the pro-	31
32	cessing of RGB video images acquired by RGB cameras or webcams.	32
33	Blood Volume Pulses (BVPs) are expected to produce changes of the in-	33
34	tensity of spectral components of the video signal [13]. In analogy with	34
35	standard PhotoPlethysmoGraphy (PPG), the term video PhotoPlethys-	35
36	moGraphy (vPPG) has been introduced. The basic steps of vPPG are	36
37	• acquiring the video signal, possibly in a specific wavelength band, and	37
38	averaging it in a region of interest to produce a time sequence reflecting	38
39	BVP changes;	39

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1	• enhancing BVPs by specific processing, and locating them, e.g. by peak	1
2	detection.	2
3	Concerning the signal acquisition, webcams [14–18] and standard video	3
4	cameras [19,13,20,21] are both used. Webcams provide low-cost and eas-	4
5	ily available setups, while standard cameras are expected to produce better	5
6	quality signals, due to higher spatial and temporal resolution, along with	6
7	multispectral imaging capabilities.	7
8	For the processing methods, a common framework is based on Blind	8
9	Source Separation (BSS) techniques modeling the video signal as a mixture	9
10	of contributions including BVP propagation, the various motion sources,	10
11	and external illumination changes. Poh et al. [14] process the RGB com-	11
12	ponent by Independent Components Analysis (ICA) to separate BVP from	12
13	other contributions. An alternative approach based on BSS by Principal	13
14	Components Analysis (PCA) was suggested by Lewandowska et al. [18].	14
15	The limitations of BSS (ICA- and PCA-based) have led several researchers	15
16	to investigate more robust processing methods able to cope with motion ar-	16
17	tifacts. Wang et al. [19] exploit image redundancy to counteract the effects	17
18	of facial movements. Feng et al. [17] adopted a simplified model of skin	18
19	optical properties to compensate for head motion. Tarassenko et al. [20]	19
20	proposed a vPPG system exploiting autoregressive modeling of video time	20
21	series to compute HR together with RR and oxygen saturation.	21
22	In general, HR estimation from vPPG is in good agreement with ref-	22
23	erence techniques (usually standard PPG or ECG in a few studies), high	23
24	correlation coefficients being reported by most authors. It is worth not-	24
25	ing that, to date, experimental results have been from small populations of	25
26	volunteers.	26
27	Though video signal intensity is the most utilized source of information,	27
28	an alternative method based on head motion related to BVP propagation	28
29	and recorded by video is reported in [22].	29
30		30
31	Heart Rate Variability	31
32	In addition to heart rate, the temporal variation of Heart Rate Variability	32
33	(HRV) is an indicator of health status in the general population, of adapta-	33
34	tion to stress in athletes [23], and of fatigue in drivers [24].	34
35	The assessment of HRV from video is usually more demanding than	35
36	simply assessing HR. In fact, while HR estimation only requires BVP de-	36
37	tection to compute the average number of pulses per minute, a precise	37
38	temporal localization of pulses is needed for HRV assessment. Most meth-	38
39	ods for HR assessment from video can be adapted to estimate HRV. For	39
	1	

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example, in [14] vPPG is used to compute the related tachogram (i.e. the
 time series of inter-beat interval duration) and to compute standard HRV
 indices both in time and frequency domain. A high correlation with the
 parameters derived by standard PPG on 15 subjects is reported. An alterna tive solution based on zero-phase component analysis has been reported by
 Iozzia et al. [25] to evaluate the suitability of vPPG for assessing autonomic
 response.

⁹ Respiratory Rate

Computer vision may support the assessment of RR and related breath-ing disorders. A recent application that may have important clinical im-pact is the assessment sleep apnea. Obstructive Sleep Apnea (OSA) is a sleep breathing disorder characterized by partial or complete obstruction of the upper airway during sleep. Left untreated, OSA has been linked to an increase in motor vehicle and occupational accidents, hypertension, cardiovascular disease, and diabetes. Since present diagnostic methods are complicated and require in-hospital stay, computer vision technologies of-fer a novel and interesting solution for diagnosing OSA [26]. Monitoring RRs has been approached by computer vision systems also related to posi-tions in bed. This aspect is particularly important for the aging population since posture changes in bed may reflect sleeping disorders; disturbances of sleep rhythm could be related to nocturnal falls, one of the most important causes of morbidity in elderly subjects.

A direct approach to video-based RR estimation is based on the analysis of chest movements. Benetazzo et al. [27] used a RGB camera equipped with a depth sensor to evaluate RR from depth data. As already mentioned, Tarassenko et al. [20] proposed a direct RR estimation from video streams by autoregressive models of video time series. Indirect approaches to RR estimation are based on the power spectrum of HRV signals: indeed, respi-ration introduces a peak in the high-frequency region of the spectrum [14].

6.3.2 Posture and Movement

In recent decades, studies of quantitative analysis of human posture and
movements have been stimulated by several fields, including rehabilitation,
sports, children's motor skills, and aging. We focus in particular on
gait analysis and fall detection;
movement for rehabilitation.

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1 Gait Analysis and Fall Detection

A relation exists between gait, cognitive decline, and risk of falls [28]. In older people, higher stages of cognitive impairment were associated with reduced ability to increase speed and walk quickly [29]. In particular, pre-venting falls in the elderly is a challenging task currently being investigated by many researchers [30]. Wearable sensors are mostly used in gait studies [31]; however, in recent years vision-based solutions have been introduced to improve unobtrusive monitoring. In this perspective, several researchers have proposed vision based systems to assist the elderly at home and reduce the risk of falls. The vast majority of reported approaches exploit standard single-view cameras with a wide field of view able to image the entire person [32-35], multiview camera-based systems [36], or omnidirectional surveillance cameras [37]; the use of depth sensors is also reported [38]. In general, the idea underlying most of these systems is predicting/rec-ognizing falls by dynamic analysis of image sequences of the monitored subject. This usually relies on a model of the observed motion coupled with the classification of the inferred activities. To obtain a compact motion description, a common choice is based on the silhouette of the monitored subject. It is usually extracted following some sort of background suppres-sion so as to reduce interference from the surrounding scene. Even though this operation can dramatically simplify the motion description, it can be prone to noise and can lead to false alarms, a matter that needs to be dealt with to achieve a reasonable system acceptability. Subject motion can be described by features extracted from the bounding box of the silhouette tracked over time. Various solutions have been proposed which include: Hidden Markov Models [39] or Layered Hidden Markov Models [36], Finite State Mod-els [35], and the use of Historical Motion Image [32,33] computed by time integration of image features possibly using eigenspace methodology to reduce dimensionality [33]. Falls can be recognized by standard machine learning methods such as multilayer perceptrons [33], algorithms based on distance between feature histograms of the silhouette bounding-box [40], and specific motion quantification coefficients [32]. As some processing steps can be prone to structured and nonstructured noise (e.g. background suppression), attempts to reduce possible inaccuracies have been faced [40]. The integration of visual and nonvisual cues (e.g. acoustic signals) has been proposed to improve fall detection accuracy [39].

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Movement for Rehabilitation

Rehabilitation is a dynamic process which allows persons to restore or at least improve their functional capability to normal. Physiotherapy exercise is a medical treatment aimed at returning patients to a normal life. During rehabilitation plans, patients may encounter difficulties such as time and cost of traveling, waiting for the availability of specialists, and ineffective personal exercise. These difficulties could be greater for those patients liv-ing in the areas that are distant from medical centers or that lack medical staff and experts, and for the frail elderly. Therefore, the concept of tele-physiotherapy has been developed to allow patients and medical experts to carry on their sessions through telecommunication networks as if they were in the same place. In general, the implementation of home-based rehabili-tation interventions is an emerging area of scientific interest and where the use of sensors plays a fundamental role.

Computer vision-based approaches in particular are expected to ease the optimization of rehabilitation strategies at home. In fact, they enable ob-jective and quantitative monitoring of physiotherapy exercises: the user's motion can be accurately tracked in 3D and compared to the planned therapy, thus enabling the fine-tuning of the therapeutic feedback on an in-dividual basis. Also, the combination of sensing technology and interactive gaming or virtual reality can facilitate the implementation of rehabilitation exercise programs [41].

One of the main fields of interest is represented by stroke survivors. Approximately 800,000 new cases of stroke are reported each year in the United States. About 80% of acute stroke survivors lose arm and hand movement skills [42]. Movement impairment after a stroke typically re-quires intensive treatment. Due to resource reduction in healthcare all over the world, in-hospital rehabilitation tends to be limited. Thus, stroke re-habilitation in home environments is an appealing solution. Computer vision systems that allow individuals with stroke to practice arm move-ment exercises at home with periodic interactions with a therapist have been developed by different research groups [43,44]. It has been demonstrated that combining telemedicine with in-home robot-assisted therapy (telerehabilitation) for people with residual impair-

ment following stroke is able to reduce barriers. Moreover, it is costeffective, providing high-quality treatment to patients with limited access
to rehabilitation centers. Interestingly, patients and caregivers report overall
satisfaction and acceptance of telerehabilitation intervention, with a marked
reduction in drop-outs [45].

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6.3.3 Anthropometric Parameters

Anthropometry is the branch of anthropology dealing with the quantitative measurement of the human body, including size, proportions, and com-position [46]. The most often used anthropometric body parameters are weight, height, skin-fold thickness, mass, triceps skin-fold, neck circum-ference, waist circumference, hip circumference, and mid-arm circumfer-ence. Derived indices such as Body Mass Index (BMI) [47], waist-to-hip circumference ratio, and waist-to-height ratio are also commonly used. An-thropometric measurements are used by the World Health Organization to describe physical trends in large-scale population studies [48,49]. Cut-off values and ranges, inferred on the basis of these statistics, are used to classify the individual status. Recently, many works have focused on cor-relating anthropometric parameters or derived indices with risk factors of cardiovascular and metabolic risk, such as overweight, obesity, and body fat distribution [50–58]. Manually collected anthropometric measurements are intrinsically af-fected by inter- and intra-observer variability; instead, computer vision technologies may support the automation and standardization of the ac-quisition, analysis, and recording of the physical parameters. Therefore, vision-based AAL solutions for the automatic computation and monitoring over time of anthropometric parameters may offer great support to longi-tudinal health studies. Nowadays, there are many devices that can acquire people's 3D shape and appearance, including low-cost depth sensors (e.g. Microsoft Kinect, Asus Xtion), whole-body scanners (e.g. Cyberware, TC^2), mixed solutions (e.g. the turnable station designed by Styku for fitness and health), portable scanners (e.g. Artec3D). These 3D scanners can capture highly accurate 3D body maps, including size, shape, and skin-surface area, in 1 to 10 sec-onds [59–63]. Standard photogrammetry has also been used to obtain a 3D reconstruction of a human body from a sequence of RGB images [64]. The above technologies provide the automatic extraction of hundreds of measurements from a body or facial reconstruction, avoiding manual measurement and transcription errors, and ensuring the repeatability of the measurements. Also, the use of acquired 3D data overcomes the 1D nature of tape measurements, by supporting volume and surface measurements, potentially meaningful with respect to the subject's overall health status. Additional resources for 3D digital anthropometry include publicly or commercially available datasets. For example, the Civilian American and European Surface Anthropometry Resource project (CAESAR) [65]

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1	dataset contains thousands of full-body textured 3D scans, labeled with	1
2	anthropometric landmarks, and supporting the study of shape spaces in	2
3	[66]. Also, several databases of human faces are available, the face being a	3
4	rich source of information about an individual's psycho-physical status. The	4
5	repositories of 3D facial data include CASIA HFB [60], FRGC v2.0 [67],	5
6	Magna Database [68], USF Human ID 3-D [69], EURECOM Kinect Face	6
7	dataset [/0], and the Basel Face Morphable model [/1].	7
8	In the following, we revised main methods to assess	8
9	• body parameters,	9
10	• face parameters.	10
12	Body Parameters	12
13	The analysis of reconstructed 3D bodies includes the surface skeleton ex-	13
14	traction: the location of feature points: the analysis of local properties	14
15	(such as curvature): and the measurement of lengths, areas, and volumes	15
16	of specific curves or regions. The registration and alignment of 3D recon-	16
17	structions with reference models is either based on the location of a very	17
18	few feature points characterized by local shape descriptors (e.g. curvature	18
19	maps [72], auto diffusion function [73], integral invariants [74], salient ge-	19
20	ometric features [75]) or on dense correspondence (e.g. multidimensional	20
21	scaling methods based on geodesic distances [76]).	21
22	The correlation between 3D shape measurements of the human body	22
23	and health issues has been studied in [77-81] in comparison with clas-	23
24	sical anthropometric measures and indices. The use of body landmarks	24
25	to perform shape measurements requires the precise location of the body	25
26	landmarks themselves [82], which can be difficult, especially in the case of	26
27	points that are poorly geometrically characterized. Therefore, many digital	27
28	anthropometry methods have focused on overcoming the precise location	28
29	of body landmarks. Recent works have focused on finding relevant correla-	29
30	tions between geometric parameters automatically computed and body fat	30
31	estimates, or cardiovascular and metabolic risk factors. Among these, Gia-	31
32	chetti et al. presented in [83] a pipeline for processing heterogeneous 3D	32
33	body scans (skeletonization and body segmentation) and extracting geo-	33
34	Another suggestation are independent of pose and robust against hoise.	34
35	Another representative example of an automatic system for the extraction	35
30 27	the Barin index is introduced and is defined as	30
37 38	the Duriw index is introduced and is defined as	رد عد
39	$Barix = \frac{\text{Torso Height } * \text{ Torso Surface Area}}{2}$.	30
	Torso Volume	55

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1	The clinical value of the index was assessed through a study of hundreds of	1
2	human scans, showing significant correlation with body fat composition.	2
3		3
4	Face Parameters	4
5	The face has always been a very rich source of information, for example	5
6	in studies on Human Computer Interaction, automatic detection of user's	6
7	feelings, and early detection of numerous diseases, such as obstructive sleep	7
8	apnea.	8
9	A number of studies have focused on using 2D images to detect mor-	9
10	phological facial correlates of body fat. In [85], Ferrario et al. observed an	10
11	increase in some facial dimensions in a study on facial morphology of obese	11
12	adolescents. Djordjevic et al. [86] reported an analysis of facial morphology	12
13	of a large population of adolescents under the influence of confounding	13
14	variables: though the statistical univariate analysis showed that four prin-	14
15	cipal components of the face (face height, asymmetry of the nasal tip and	15
16	columella basis, asymmetry of the nasal bridge, depth of the upper eyelids)	16
17	correlated with insulin levels, the regression coefficients were weak and no	17
18	significance persisted in the multivariate analysis. In [87], Lee et al. pro-	18
19	posed a prediction method, based on BMI, of normal and overweight for	19
20	adult females using geometrical facial features extracted from 2D images.	20
21	The features include Euclidean distances, angles, and facial areas defined	21
22	by selected soft-tissue landmarks. The study was extended in [88] focus-	22
23	ing on the association of visceral obesity with several facial characteristics.	23
24	The authors determined statistically the best predictor of normal waist and	24
25	visceral obesity among the considered facial characteristics. Cross-sectional	25
26	data were obtained from a population of over 11 thousand adult Korean	26
27	Description 2D data have started to be used. One of the first needle one	27
28	Recently, 5D data have started to be used. One of the first results con-	28
29	by Banabilh at al. in [80], the authors showed that granifacial obseity as	29
30	by Danadhin et al. In [69], the authors showed that cranioracial obesity, as-	30
31	appea syndrome. In [90] Ciorri et al. defined a shape descriptor based	31
32	on the theory of persistent homology and tested it on a synthetic dataset	32
33	of 3D faces to assess the relation of facial morphology with obesity and	33
34	overweight	34
35	over weight.	35
36	634 Emotions Expressions and Individual Wellness	36
37		37
38	I he intertwining of emotional states and the onset and progression of dis-	38
39	eases has been under investigation for a long time [91]. Studies in modern	39

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neuroscience have shed new light on the topic, leading to an extended reconsideration of the classical view of the interaction of soma and psy-che [92]. On the one hand, chronic adverse emotional states, such as stress, anxiety, and tiredness, are among the main risk factors of serious ill-nesses, including metabolic syndrome and cardiovascular diseases [93-95]; conversely, the effect of positive states may reduce the incidence of cardio-vascular disease [96]. On the other hand, chronic illness is coupled with an emotional dimension that can affect therapy outcome; for example, dis-tress, depression, and anxiety may reduce one's motivation to access medical care and follow treatment plans [97]. Also, many studies have investigated the relation between adverse affective states (stress and depression) and the response of the immune system [98,99]. It is therefore not surprising that there is a great deal of interest in the medical community for novel tools that can assist the individual in self-managing stressful and anxiogenic situations and reducing disease risks. Computer vision may support the implementation of unobtrusive, con-tinuous monitoring systems of the emotional state of an individual, not only by supporting the estimation of emotion-related physical parameters (e.g. HR and RR; see Section 6.3.1), but also by analyzing facial expressions and body language evoked by emotions [100]. Indeed, assessing individ-ual psychological wellness implies the recognition of complex mental states such as fatigue, frustration, pain, depression, and mood, which require the integration of multiple cues: physiological, acoustic, and visual cues. The combined use of physiological parameters computed by sensors and expres-sive features is documented in [101]. The visual clues to the affective state include general facial expression, micro-expressions, and other features such as eye gaze and head orienta-tion. In general, the interpretation of facial codes in terms of underlying emotional states remains an open problem. Coding schemes such as the Facial Action Coding Scheme (FACS) [102] are generally related to pri-mary affective states (e.g. anger, fear, happiness) rather than to complex states. Additional information about complex states may derive from micro-expressions, which are brief (lasting between 1/25 and 1/3 of a second) low-intensity facial expressions believed to reflect repressed feelings [103]. Due to their subtlety, they are hard to detect; for this reason the use of local dynamic appearance representations extracted from high-frequency video is usually reported [104]. The video-based analysis of multiple visual clues, including head, eyebrows, eye, and mouth movements, led in [105] to a technique for the identification of stress and anxiety.

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For a detailed analysis of computer vision techniques for affective state recognition, we point the reader to Chapter 10 of this book. Here we con-fine ourselves to observing how moving emotional analysis in AAL settings is an exciting though extremely challenging task, which can pursue the objective of assessing emotional wellness. In particular, at-home monitor-ing can be implemented to evaluate stress, fatigue, and anxiety in different conditions, including resting states and a wide variety of everyday tasks (e.g. watching TV, listening to music, using a PC, or doing homework), which should ensure a detailed and possibly complete description of the individual responses to many external stimuli. In addition, AAL favors the correlation of monitoring data with life-style habits. This can be the key towards a true holistic representation of individual wellbeing in naturalistic contexts. 6.4 METHODOLOGICAL, CLINICAL, AND SOCIETAL **CHALLENGES** We have seen how computer vision holds the potential to boost a new gen-eration of noninvasive, effective systems for continuous health monitoring. The possibility of close follow-up by means of technological solutions at home would be an additional time-saving support to busy health profes-sionals. These tools could help physicians not only in managing chronic diseases, but also in counseling on risk factors in the general population, especially for primary prevention. To make this scenario come true, some methodological, technological, clinical, and societal challenges still need to be faced. **Computational Demand** In physiological monitoring, high computational demand could result from the need to acquire and process data in real time, including real-time tracking, data alignment, and data analysis. Also, the spatial and tempo-ral resolution of the acquisition may be high, depending on the parameters to be computed; the resolution requirements should be balanced with com-plexity and cost requirements, depending on the application at hand. Acquisition Robustness in Real-Life Scenarios Acquiring physiological parameters in uncontrolled settings requires meth-ods that are robust to occlusions, clutter, or pose, for example the presence of a beard or make-up while analyzing the facial skin, or slight move-ments of the user while recording vital signs. Also, robustness to lighting

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1	conditions can be an issue in several applications, and computer-controlled	1
2	external light sources may be required.	2
3	To operate in real-life scenarios, it is also mandatory to capture data	3
4	without requiring too much effort from the subject, i.e. without asking the	4
5	subject to stay still in front of a camera for several minutes. The challenge	5
6	here is how to automate the acquisition process so that data are captured	6
7	when the environmental conditions are most favorable.	7
8		8
9	Reliability of Measurements for Clinical Purposes	9
10	It is mandatory that physiological monitoring systems provide a description	10
11	of the individual status coherent with the clinical view. In particular, a cru-	11
12	cial requirement is the reliability of measurements and their usability by	12
13	doctors and health professionals. Even though it is not expected that moni-	13
14	toring systems produce results in the form of validated clinical tests, the data	14
15	provided must be adequate to properly drive the physician's reasoning and	15
16	action planning. This requires intelligent image processing algorithms, en-	16
17	suring high repeatability, adequate sensitivity, and specificity in measuring	17
18	data in comparison to standard reference methods used in clinical practice.	18
19		19
20	Clinical Evaluation	20
21	Evaluating and validating in-home monitoring systems is a nontrivial task	21
22	that requires an interdisciplinary team and a close involvement of the med-	22
23	ical experts. The validation issue also calls for shared benchmark datasets.	23
24	The literature reports few and small case studies, which means that	24
25	new studies involving a greater number of subjects become mandatory.	25
20	In the particular case of physiological monitoring, satisfactory clinical ev-	20
27	idence should be provided regarding the reliability of measurements, and	27
20	also regarding the improvement in the quality of life, wellness, and health	20
29	conditions brought by technological solutions.	20
31	6 7 8	30
32	Acceptability and Long-Term Engagement	32
33	To be applicable on a large scale, video-based assistive technologies must be	33
34	accepted by the end users including monitored subjects their families and	34
35	carers	35
36	Stimulating initial adoption of the technology and long-term engage-	36
37	ment is the key to making a true impact in real-life scenarios. To this end	37
38	the monitoring system design should adapt to different scenarios that range	38
39	from primary prevention for healthy youngsters to the management of	39
	really prevention for neurony youngsters to the management of	

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1	chronic diseases in the elderly. While the physiological parameters com-	1
2	puted could be the same in these scenarios, the best way to acquire data,	2
3	interact, and communicate should be tailored to the specific needs of the	3
4	users and their carers.	4
5		5
6	Privacy and Security	6
7	The monitoring of sensitive physiological data bears with it the issue of	7
8	privacy. On the one hand, people should be made aware of a functioning	8
9	system in order to augment their sense of trust and confidence and the	9
10	feeling that they are retaining control of their data. On the other hand,	10
11	cross-age and cross-gender studies are needed to assess individual levels	11
12	of user acceptance since the concept of privacy is evolving as technology	12
13	evolves [106] and the perception of privacy shows cultural, gender, and age	13
14	differences. The goal is to support the development of privacy-by-design	14
15	video-based systems, which take into account user privacy requirements	15
16	from the very beginning [107].	16
17	Another issue is that sensitive data can be intercepted by third parties	17
18	and used for malicious purposes. The recording of images and video data	18
19	makes preventing sensitive data from attacks especially urgent. The problem	19
20	of cyber-security calls for solutions from different fields, including cryptog-	20
21	raphy, data management, data mining, and related areas.	21
22		22
23	6.5. A DOSCIPLE COLUTION: THE WIZE MIDDOD	23
24	0.5 A POSSIBLE SOLUTION: THE WIZE MIRROR	24
25	The European Community's Seventh Framework Programme Project SE-	25
26	MEOTICONS developed an innovative AAL solution that extensively	26
27	leverages computer vision methods into a noninvasive device for wellbeing	27
28	monitoring. The multisensory device, which looks like a common mirror	28
29	and is called the Wize Mirror, was conceived as an effective technology-	29
30	assisted intervention to prevent cardiometabolic diseases.	30
31	Cardiometabolic diseases (i.e. cardiovascular diseases and type 2 dia-	31
32	betes) are the leading causes of mortality worldwide and their spread on a	32
33	global scale is putting a strain on social resources and health systems. An	33
34	estimated 17.7 million people died from cardiovascular diseases in 2015,	34
35	corresponding to 31% of all global deaths [108]. This figure is expected to	35
36	increase in the coming years due to population aging and the increasing in-	36
37	cidence of obesity and diabetes [109]. Clinical evidence has demonstrated	37
38	that the majority of cardiometabolic diseases can be prevented by limit-	38
39	ing exposure to the main risk factors; by exercising regularly, eating well,	39

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1 2 3 4	controlling stressful conditions, avoiding smoking, and moderating alcohol intake, about 90% of type 2 diabetes, 80% of coronary heart disease, and 70% of strokes could be prevented [110]. This awareness has fostered the promotion of advectional and guidance programs for lifetule improvement	1 2 3 4
5 6	that call for assistive and personal technologies as a powerful ally to address	5 6
7 8 9 10 11 12 13	The Wize Mirror responds to this call coming as a self-monitoring de- vice able to blend seamlessly into life's daily routines. The guiding principle was to have a device able to minimize invasiveness, obtrusiveness, and at- tention theft, while maximizing usability, trustfulness, and user acceptance. This appears, in fact, to be the most promising way to address and engage various shares of the at-risk population, who have assorted needs and ex- pectations and have diverse digital skills. The Wize Mirror implements an	7 8 9 10 11 12 13
14 15	AAL solution based on a virtuous cycle underpinning three main elements:	14 15
16 17 18	 sen-measurement, education and coaching; user experience, with particular emphasis on contact with healthcare 	16 17 18
19 20	professionals. Combining together these features into a loop has demonstrated to be	19 20
21 22 23 24 25	the key to ensuring the acceptance, effectiveness, and long-term impact of self-monitoring AAL interventions [111]. The Wize Mirror blends to- gether these functionalities by taking into account the diverse challenges reported in Section 6.4.	21 22 23 24 25
26	6.5.1 Self-Measurement	26
27 28 29 30 31 32 33 34 35 36 37 38	The Wize Mirror seamlessly integrates a contactless sensing framework, including different types of cameras, and a data processing platform able to scan the person in front of it and assess physiological markers of car- diometabolic risk. The main cardiometabolic risk factors include hyperten- sion; dyslipidemia; glucose dysmetabolism; obesity and overweight; noxious habits such as smoking and alcohol abuse; and adverse psychological states such as chronic conditions of stress, anxiety, and fatigue [108]. Stemming from the principles of medical semeiotics [112], the Wize Mirror analyzes physical and expressive traits of the face and the composition of the breath to detect both perceptible and subtle signs correlated to the factors listed above. The sensing framework relies on	27 28 29 30 31 32 33 34 35 36 37 38
39	• an inexpensive 3D scanner based on depth cameras;	39

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1	and prototyping trials that explored several options with respect to the user	1
2	position in front of the Mirror. This was done to achieve the best view and	2
3	overcome disturbances. Similarly, the lighting system was devised to coun-	3
4	teract ambient light disturbances and ensure the homogeneous illumination	4
5	of the face during data acquisitions.	5
7	3D Data	7
8		8
9	The SD scanner data are processed to enable	9
10	• face detection and recognition, used to detect and recognize the user in front of the Mirror, as reported in [114]:	10
11	• 3D head nose tracking, facial segmentation, and labeling:	11
12	 3D reconstruction 	12
13	These are core functionalities that serve as a common asset for the	13
14	other data processing facilities of the Mirror. The 3D data are in fact used	14
15	to enable face detection and labeling on the 2D data obtained from the	15
16	other camera systems. This choice responds to the need for robustness and	16
17	efficiency of data processing methods. Face detection and tracking is per-	17
18	formed on the data from the depth sensors only once rather than several	18
19	times on the various data streams: this ensures robustness to varying illu-	19
20	mination conditions and optimizes the processing time. The user is first	20
21	detected in the 3D space; then, by fitting a face mask on the depth sensor	21
23	data, the position and the orientation of the user's face are detected. After	23
24	that, selected facial landmarks are localized and their 3D coordinates are	24
25	projected into the 2D frames of the other camera streams. This is done by	25
26	using the intrinsic and extrinsic parameters of the cameras within a camera	26
27	calibration and registration procedure done at system setup [113]. The cam-	27
28	era's synchronization procedure allows the system to meet the requirement	28
29	for real-time processing.	29
30	The 3D model of the face serves the anthropometric and morphometric	30
31	analyses. It results from a reconstruction algorithm adapted from the Kinect	31
32	fusion method to meet the needs posed by the fact that in the Mirror	32
33	the depth sensors remain in a fixed position while the face is moving [7].	33
34	A re-mesning algorithm runs on the 3D point cloud to ensure producing a	34
35	manifold, without holes and degenerate elements [115].	35
36	Facial Morphometry	36
37 38	Easial mombamatery analyzes the 2D face model to detect sizes which it	37
30	avery analyzes the SD face model to detect signs related to	20
	overweight and obesity. Four snape parameters are computed on the 5D	59

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in the blood, which is one of the signs of dyslipidemia. In the Mirror, they are detected and measured on images acquired on a single wavelength (560 nm or 580 nm) by estimating the droplets with higher skin reflection in an area underneath the eye (where fat accumulates most) [113]. AGE-products are linked to the metabolism of glucose. Their accumu-lation in the skin increases with aging, but when above a certain threshold, it signals an increased risk of cardiometabolic disorders. In the Mirror, AGE accumulation is estimated during UV exposure from a 365 nm LED as the ratio of the fluorescence intensity (evaluated on a 475 nm image) to the illumination intensity (evaluated on a 360 nm image). See [117] for further details. The analysis of skin function aims to assess endothelium function. The endothelium regulates vasodilation in response to different blood-flow needs. A dysfunction of this tissue may be a consequence or a cause of several pathologies, such as hypertension, hypercholesterolemia, and di-abetes. In the Mirror, endothelial function is measured on MSI data by assessing the response of facial skin microcirculation after heating the cheek via a computer-controlled remote skin heater. An index of the function is defined based on two parameters calculated on 475-650 nm images: hemoglobin oxygenation and the fraction of red blood cells in the skin before and after heating [113]. Vital Signs and Emotional Cues By processing 2D videos, the Mirror estimates vital signs and emotional cues connected to adverse psychological statuses. Vital signs include HR, RR, and HRV, which are indeed the most informative parameters associ-ated with the psycho-physical status of an individual. In the Mirror these parameters are analyzed through video-processing methods based on blind source separation through Independent Component Analysis, as described in [118]. Cues of emotional status derive from the analysis of short video record-ings processed to spot micro-expressions and facial gestures typical of stress, anxiety, and fatigue. For stress and anxiety, these cues generally corre-spond to facial-muscle hyperactivity, which may be discretized in head movements, eye movements (in terms of eye gazing and frequent focus, pupil dilation, and blinking rates), and mouth movements (in terms of jaw clenching, lip trembling, and biting). Fatigue is here intended as a sense of tiredness, lack of energy, and a feeling of exhaustion. Signs of fatigue are mainly yawing and saccadic movements. In the Mirror, all these signs

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are extracted from the videos though different feature extraction methods
and are fed into an Artificial Neural Network model trained to classify
emotional traits [113,105]. Considering how challenging and complex a
proper recognition is, the neural model also takes in vital signs (i.e. HR
and RR) and uses as reference a video shot at baseline during the user's
registration when the user is shown a video to induce a relaxed condition.

9 Breath Analysis

The gas sensing device connected to the Mirror analyzes the composition of the breath and supplies feedback about the effect of noxious habits. The device, called the Wize Sniffer, detects molecules such as carbon monoxide, ethanol, hydrogen, oxygen, and carbon dioxide. The presence and variation of these substances can be correlated to smoking, alcohol consumption, and metabolic disorders. The Sniffer acquires a breath sample through a corrugated tube connected to the Mirror, analyzes its composition and provides the Mirror with a grading of the risk the users are exposed to due to their habits (no risk, moderate risk, or high risk) [119].

Acquisition Timing

The Mirror requires just a few seconds without requiring too much effort to scan the faces of the users while they are standing or sitting in front of it as part of their daily routine. Overall, facial morphometry, skin composi-tion, vital signs, and emotional analyses all together take one minute of data acquisition. Breath analysis takes the time of a deep breath and it entails the simple interaction of breathing into a mouthpiece. Thanks to a paral-lel implementation on a multiprocessor board, results are provided in real time, in only a few seconds. Only HRV and endothelial function require a five- and six-minute acquisition, respectively. This time is unavoidable and is necessary to ascertain the dynamics of the underlying physiological phenomenon. It is worth underlining that unlike the breath analysis, all the other analyses rely on image and video processing. This means that they can

be integrated, with proper customization, into any device or equipment that already hosts or is able to host some of the sensors behind the Mirror such as a TV set, a mobile phone or tablet, a personal computer, etc. This flexibility increases the potential of the Wize Mirror to address users with different needs and preferences.

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6.5.2 Education and Coaching

The Wize Mirror is an interactive device with a touchscreen Graphical User Interface (GUI) that conveys information to and from the users. Through the GUI, the Mirror trains on and guides the users through the self-measurement procedure and informs them about the significance of the parameters measured. It also provides the users with high-quality educational materials on cardiometabolic risks and the importance of pri-mary prevention. In the current implementation, during data acquisition, the Mirror displays some short and sharp messages promoting behavioral changes, complementing them with captivating and instructive images or short videos. Although properly explained, the set of measurements that the Mir-ror is able to assess covers a wide range of psycho-physiological parameters that if displayed separately may overwhelm the users and mislead their un-derstanding of their own status. To avoid this, the Mirror integrates the measurements into a Wellness Index, which measures the users' wellness with respect to the risk of a cardiovascular disease on a scale from 1 to 100. The Index results from the application of a Structural Equation Model [120] to the measurements taken by the device and other data inputted by the users through validated questionnaires on their habits and attitudes [113]. The Index is displayed on the Mirror (see Fig. 6.3), organized in three main components that cover the main facets of individual wellness: (i) the physical component summarizes the physical conditions of the user as the outcome of physiological measurements (i.e. facial morphometry and skin composition and function); (ii) the emotional component measures psy-chological conditions as a combination of the emotional cues and the vital signs; and (iii) the lifestyle component scores the users' habits in terms of noxious habits, diet, and physical activity by leveraging outcomes from the Sniffer and the data provided by the questionnaires. The approach behind the WI is highly innovative, since it merges objective measures (obtained by the device) with subjective information provided by the users on their perceived status. Other solutions currently in use, such as the WHO-5 in-dex [121], use only the subjective evaluation and this can obviously hide potential biases. As shown in Fig. 6.4, the Wellness Index is traced over time and stored in the Mirror in a diary to be consulted by the users. Its evolution over time

is the basis of the personalized guidance that counsels the users on lifestyle
 improvements that increase their WI and ameliorate their physical and emo-

³⁹ tional health. The guidance relies on the definition of the user profile in ³⁹

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quality information based on scientific evidence is becoming more and more urgent and mandatory. Overall, educational and counseling messages contribute to improving users' knowledge and risk perception, ameliorat-ing their health literacy, and increasing their involvement and degree of comfort in making healthy choices [122]. The approach adopted by the Wize Mirror stems from these consider-ations and is meant to captivate the users by offering a holistic approach to wellness. As a matter of fact, more and more people are seeking ways not only to lose weight or look better, but also to improve their quality of life and overall sense of wellness. 6.5.3 User Experience A pleasant user experience is crucial to stimulating the initial adoption and periodic utilization of self-monitoring devices. The Wize Mirror features a touchscreen and an intuitive interface that makes it usable and appealing to people with different digital skills. It also offers a range of user applications and services that span from sharing data with healthcare professionals and general practitioners to playing music, social network connections, email consultation, and web surfing. The Wize Mirror can indeed be seen as a big tablet integrated into the bathroom mirror. Future extensions include the connection to wearable devices or mobile apps to automatically upload data on physical activity, sleep, and diet. Among the different services, the link with healthcare professionals is of paramount importance: on the one hand, it reinforces the impact of the device by making the users feel more secure and cared about; on the other hand, it enables care providers to gather data and insight never available before. To meet privacy and security requirements, the Mirror features an au-thentication facility that is based on the automatic user recognition, but it always requires a confirmation code. A privacy-by-design approach was adopted to design the storage system along with data encryption. The data shared with care professionals mainly consist of the Wellness Index and measurement values. Images and videos are never transferred from the Mir-ror over the Internet. 6.5.4 Wize Mirror Validation The Wize Mirror underwent a validation campaign to verify the accuracy, repeatability, reproducibility, and effectiveness of its measurements and to

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check acceptability by the users. Three prototypes were deployed in three clinical sites in Italy and France between July and October 2016. A human study involved 72 volunteers who underwent Mirror scans every 15 days for three months. Reference data were acquired contextually with diag-nostic devices used in clinical practice to measure body composition and metabolic, homeostatic, and vital parameters. A comparison showed a statis-tically significant correlation of Mirror measurements and standard clinical measures. Moreover, it was observed that both originally motivated and unmotivated volunteers were able to significantly modify their physiologi-cal conditions, and that there was an evident decrease in their BMI. Details on these outcomes are being reported in a dedicated paper to be published within the medical literature. Overall, the validation demonstrated the reliability of the Mirror's mea-surements and interventions. This is key to nurturing the device acceptance by both the end users and the clinical professionals. In particular, the clin-icians' trust in the device plays a key role in the promotion of the Mirror among the at-risk population. 6.6 CONCLUSION In recent decades healthcare systems have experienced an exponential growth in costs that is related to different social, cultural, and economic fac-tors. The need for sustainable healthcare systems translates into challenges in ICT for the implementation of autonomous and proactive healthcare services. We believe the synergy between AAL technologies and computer vision may support moving medical and healthcare services from hospitals to home environments, thus cutting down healthcare costs. As observed in [2], AAL systems could support the third generation of telecare systems. The first generation was the panic-alarm gadgets used to summon help in case of emergency, and the second was sensor-based monitoring systems used to support medical decisions; the third genera-tion of systems shifts from a reactive approach to a proactive strategy for anticipating emergency situations. Computer vision can help embark on this revolutionary path. Science and technology and research are mature, though further research is needed to solve a number of open issues, includ-ing robustness, accuracy, and nonintrusiveness of data acquisition; clinical validity of the output delivered by existing techniques; and attention to the needs and demands of real end users in terms of acceptability and long-term engagement.

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1	With the Wize Mirror, we have seen how we can begin to think of	1
2	a fourth generation of telecare systems, which are explicitly designed to	2
3	influence human behavior and persuade people to act upon their lifestyles	3
4	and their health. We believe the convergence of different disciplines, from	4
5	information technology (including computer vision) to cognitive science,	5
6	is the way forward.	6
7		7
8		8
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15	cashire) for their valuable contributions to the development of the Wize Mirror.	15
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