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Abstract Medical image classification using convolutional neural networks (CNNs) is promising but often

requires extensive manual tuning for optimal model definition. Neural architecture search (NAS) automates this process, reducing human intervention significantly. This study applies NAS to [18F]-Florbetaben PET cardiac images for classifying cardiac amyloidosis (CA) sub-types (amyloid light chain (AL) and transthyretin amyloid (ATTR)) and controls. Following data preprocessing and augmentation, an evolutionary cell-based NAS approach with a fixed network macro-structure is employed, automatically deriving cells' micro-structure. The algorithm is executed five times, evaluating 100 mutating architectures per run on an augmented dataset of 4048 images (originally 597), totaling 5000 architectures evaluated. The best network (NAS-Net) achieves 76.95% overall accuracy. *K*-fold analysis yields mean \pm SD percentages of sensitivity, specificity, and accuracy on the test dataset: AL subjects (98.7 ± 2.9 , 99.3 ± 1.1 , 99.7 ± 0.7), ATTR-CA subjects (93.3 ± 7.8 , 78.0 ± 2.9 , 70.9 ± 3.7), and controls (35.8 ± 14.6 , 77.1 ± 2.0 , 96.7 ± 4.4). NAS-derived network performance rivals manually determined networks in the literature while using fewer parameters, validating its automatic approach's efficacy.

Keywords (separated by '-') Neural architecture search - AutoML - Nuclear medicine - [18-F]-Florbetaben - Cardiac amyloidosis

Footnote Information Filippo Bargagna and Donato Zigrino contributed equally to this work.



Automated Neural Architecture Search for Cardiac Amyloidosis Classification from [18F]-Florbetaben PET Images

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Abstract

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Keywords Neural architecture search · AutoML · Nuclear medicine · [18-F]-Florbetaben · Cardiac amyloidosis

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Introduction

Machine learning (ML) is a discipline that supports radiologists in the development of new biomarkers and better analysis of medical images towards accurate diagnosis. Among ML techniques, deep learning (DL) provides powerful methods for classification, segmentation, and recognition of medical images [1, 2]. DL is based on algorithms relying on Neural Network (NN) structures, made of several interconnected nodes, also known as neurons, that process information and automatically extract features from unstructured data [3].

NN, in general, are comprised of three main types of layers, each one composed of several nodes: the input layer, which receives data and passes it to the rest of the architecture; the hidden layers, which apply non-linear functions to the data; the output layer, that provides processing results under various formats depending on the task at hand (regression, classification).

Convolutional neural networks (CNN) are a sub-type of NN, having as hidden layers three specific ones:

Materials and Methods

Theory

Neural Architecture Search

NAS focuses on optimizing the topology of an architecture, usually portrayed through a directed acyclic graph (DAG), where neural network operations label the nodes or edges. NAS methods are typically categorized according to three dimensions: 1. The *Search Space* \mathcal{A} refers to all possible architectures that can be used for a given task; 2. The *Search Strategy*, which explores the search space by selecting a single architecture $\alpha (\in \mathcal{A})$; and 3. The *Performance Estimation Strategy*, that evaluates the model's predictive performance on unseen data and can be done, for example, using the classic training and validation approach on the data. Figure 1 gives a synthetic description of the NAS workflow followed in this work.

convolutional layer, pooling layer, and fully connected layer. When using CNNs for classification tasks, convolutional and pooling layers extract features and information and feed them to the fully connected layers. These final layers, in turn, give class scores for the images. Designing and finding an appropriate neural network, a CNN in particular, can be a challenging task; in fact, most of the advances in neural network models usually require considerable hand-tuning of the neural network architecture, which is time-consuming and error-prone. Often, modifications to existing architectures are made using transfer learning, but their effectiveness is very much linked to the experience and knowledge of the researcher [4].

In recent years, auto machine learning (AutoML) has been developed to fulfill two main goals: automate the learning process from data pre-processing to model evaluation and make deep learning accessible to non-experts. An example of AutoML is neural architecture search (NAS) [5], which uses automated algorithms and techniques to find architectures that can achieve high performance while minimizing the need for manual trial-and-error. The process involves exploring a large search space of possible architectures and hyperparameters to find the most suitable configuration for the given problem.

The first NAS methods relied on reinforcement learning [6] and evolutionary learning [7] approaches, which achieved the best classification accuracy in image classification. This novel methodology has been used to accomplish some medical tasks, such as classifying skin lesions [8] or segmenting medical images for surgery planning and computer-aided diagnosis [9].

However, as far as we know, there are no studies regarding the application of this technique to the classification of nuclear medicine images, positron emission tomography (PET) in particular. This research aims to fill this gap by adopting and implementing the NAS-based evolutionary algorithm for cardiac amyloidosis (CA) classification from early acquired [18F]-Florbetaben PET images. Given a dataset that includes PET images from subjects with both light chain amyloidosis (AL) and transthyretin amyloidosis (ATTR) sub-types of CA as well as control subjects, the NAS methodology used in the present work is shown to automatically develop and evaluate the optimal network for the classification of the three data classes.

A comparison is also made with a CNN network already present in the literature, named CAclassNET [10], built with the classic methodology of manually finding an optimal network for classification through numerous hand-tuning phases of the parameters present in the network.

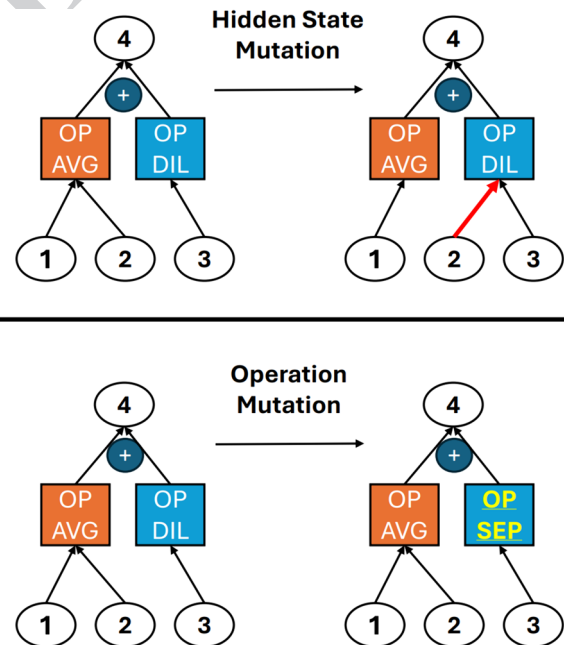


Fig. 1 Visual representation of hidden state and operation mutations inside a cell. Hidden state mutation (top): hidden state 2 connection to operations is changed; Operation mutation (bottom): the convolutional dilatation operation (OP DIL) is changed into a convolutional separable operation (OP SEP), the average pooling (OP AVG) is left unchanged

107 **Search Space**

108 A search space is the set of all architectures that the NAS
 109 algorithm is allowed to select. Common NAS search spaces
 110 range in size from a few thousand to over a billion architec-
 111 tures. Let us consider a NN as a function that, by applying
 112 operations to input variables x , produces output variables y .
 113 We can formalize it as a DAG with a set of nodes $\{z^{(1)}, z^{(2)}, \dots$
 114 $, z^{(k)}, \dots\} = Z$. Let O be a set of operations, each node $z^{(k)}$,
 115 except for the first one that is considered the input node, is
 116 a tensor evaluated as follows:

$$117 \quad z^{(k)} = o^{(k)}(I^{(k)})$$

118 with $I^{(k)}$ inputs from the sets of parent nodes and $o^{(k)} (\in O)$
 119 operation applied to nodes. The main operations, as per
 120 [11], are convolutions, pooling, activation functions, con-
 121 catenation, addition, etc. Once all the possible operations
 122 are defined, the search space can be considered either as a
 123 whole or not, giving, respectively: 1. Global search space
 124 or 2. cell-based search space. A chain and a hierarchical
 125 structure are also possible but not of interest for this work.
 126 In a global search space approach, NAS algorithms find
 127 all the components required for the entire neural network;
 128 consequently, the search space is large because the graph
 129 represents the entire network down to the single operation.
 130 Instead, in a cell-based search space approach (the one
 131 used in this work), the network is subdivided into several
 132 cells [12] with different hyperparameters (e.g., the number
 133 of filters in the first cell can be different from the number
 134 of filters in the second one). This second approach was pro-
 135 posed because many handcrafted architectures consist of
 136 repetitions of fixed structures called cells or blocks, which
 137 can be represented by a DAG. In this case, the network
 138 macro-architecture is manually defined [5], while the NAS
 139 approach is reserved for the micro-architecture inside each
 140 cell. Usually, two kinds of cells are stacked together repeti-
 141 tively: the *normal cell* that preserves the dimensions of the
 142 input; the *reduction cell* that reduces the spatial dimensions
 143 of the input.
 144

145 **Search Strategy**

146 A search strategy is an optimization technique used to find
 147 a high-performing architecture in the search space. Once
 148 the search space has been defined, it is important to explore
 149 it using suitable approaches. There are generally two main
 150 categories of search strategies: the black box optimiza-
 151 tion-based techniques (including multi-fidelity techniques)
 152 [13, 14], and the one-shot techniques [15]. However, there
 153 are some NAS methods for which both or neither cate-
 154 gory applies. Once the search space has been defined, it is

important to explore it using suitable approaches. The NAS
 problem can be defined as follows [11]: Let D be the space
 of all datasets, M the space of all deep learning models, and
 A the architecture search space, then a general deep learning
 algorithm Λ is defined as follows:

$$\Lambda : D \times A \rightarrow M$$

In this setting, an architecture $\alpha \in A$ defines the net-
 work's topology, parameters, hyperparameters, and regu-
 larization. Let $d \in D$ be a dataset, which is split into a
 training and a validation set ($d_{\text{train}}, d_{\text{validation}}$), the algorithm
 estimates the model $m_{\alpha, \theta} \in M_{\alpha}$ by minimizing a loss func-
 tion L with a regularization term R :

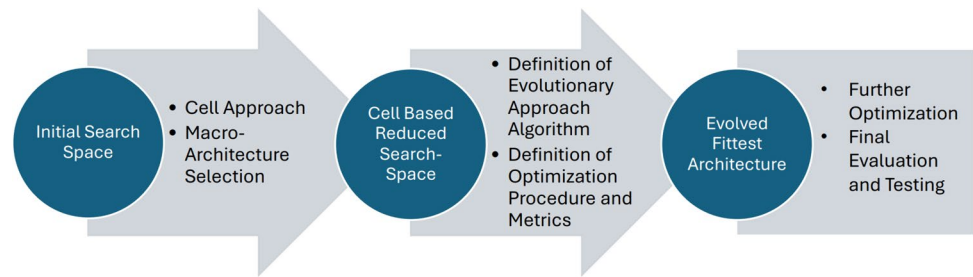
$$\Lambda(\alpha, d) = \arg \min_{m_{\alpha, \theta} \in M_{\alpha}} \mathcal{L}(m_{\alpha, \theta}, d_{\text{train}}) + R(\theta)$$

NAS has the task of finding α^* which maximizes an
 objective function $f(\alpha)$ of the validation partition $d_{\text{validation}}$.
 For example, considering the classification task, $f(\alpha)$ is
 usually the validation accuracy:

$$\alpha^* = \arg \max_{\alpha \in A} f(\alpha)$$

Here, the function f is considered only dependent on
 α as all the other settings are considered fixed during the
 NAS procedure. Several approaches exist in literature to
 explore the search space, such as random search, rein-
 forcement learning [6, 16], gradient-based optimization
 differentiable ARchiTecture search (DARTS) [17], and
 evolutionary algorithms [7]. Evolutionary algorithms use
 the essential components of a genetic optimizer to find the
 best neural network [7, 18, 19]. The approach described
 in [19] and used in the present work requires the defini-
 tion of a set of primary operations and mutation rules; the
 overall macro-architecture is also predetermined. Each
 architecture consists of a sequence of normal cells (in
 a stack of N cells) and reduction cells. For each stack
 of normal cells, the number of convolutional filters is
 equal to F ; this number is then doubled after each reduc-
 tion cell. The goal of this algorithm is to find the best
 reduction and normal cells (micro-architecture). Then, the
 search strategy works as follows: after an initial selec-
 tion of P architectures, each consisting of a repetition
 of normal and reduction cells, the validation accuracy is
 evaluated by training each model from scratch. After, the
 evolution algorithm is applied. With C as the number of
 generations (number of steps of the evolutionary algo-
 rithm), a sample of S models is randomly selected with
 replacement. The model with the highest accuracy among
 the S selected samples is then picked as the parent and
 mutated. The following three mutation rules are chosen
 according to [19]:

Fig. 2 The Neural Architecture Search workflow



- 205 1. *Operation mutation*: once a cell and a pair of hidden
 206 states are selected, one of the two operations is changed
 207 (probability: 0.475).
 208 2. *Hidden state mutation*: once a cell and a pair of hid-
 209 den states are selected, one of the two hidden states is
 210 changed (probability: 0.475).
 211 3. *Identity mutation* (in which nothing changes) is also pos-
 212 sible but with a lower probability (0.05).

213 At each step, a mutation is randomly selected and then
 214 applied to a specific cell (normal or reduction) (Fig. 2).
 215 The offspring is then trained, and its validation accuracy
 216 is evaluated. The oldest model is then removed from the
 217 population to keep the size P constant.

218 To speed up the search, the different architectures are
 219 trained for a smaller number of epochs. Then, only a subset,
 220 consisting of the best models, is selected, eventually aug-
 221 mented (by increasing N and/or F), and trained for a higher
 222 number of epochs.

223 Performance Estimation Strategy

224 A performance estimation strategy is any method used to
 225 quickly predict the performance of neural architectures to
 226 avoid fully training the architecture. For example, while
 227 we can run a discrete search strategy by fully training and
 228 evaluating architectures chosen throughout the search, using
 229 a performance estimation strategy such as learning curve
 230 extrapolation can greatly increase the speed of the search.
 231 During the search process, it is necessary to evaluate the per-
 232 formance of the candidate architecture. The easiest approach
 233 that can be used is training a neural network from scratch
 234 and evaluating its performance on the validation set. Since
 235 this approach is computationally heavy and requires a lot of
 236 GPU time, different approaches are proposed in the literature
 237 to speed up the performance estimation [5]. One of the most
 238 used methods that we used in the present work is the *lower*
 239 *fidelity estimates*, consisting of estimating the performance
 240 of the network from the learning curve trained for fewer
 241 epochs and from the relevant hyperparameters [20, 21].

Image Data

Cardiac Amyloidosis Diagnosis

242 CA is a cardiomyopathy associated with the deposition of
 243 protein fibrils in the extracellular space of the heart [22].
 244 Several types of amyloidosis can usually be distinguished.
 245 The most relevant in cardiac amyloidosis are immunoglobulin
 246 light-chain amyloidosis (AL) and transthyretin-related
 247 amyloidosis (ATTR). The main problem of this disease is
 248 that the early clinical symptoms can be confused with other
 249 conditions such as hypertensive heart disease or heart hyper-
 250 trophy secondary to aortic valve stenosis. Moreover, these
 251 two subtypes of amyloidosis require different therapies: AL
 252 patients are usually treated with chemotherapy or stem cell
 253 transplantation, while ATTR patients are subjected to small
 254 RNA-silencing molecules or stabilizers [23, 24]. There-
 255 fore, it is very important not only to diagnose the presence
 256 of amyloidosis as soon as possible but also to be able to
 257 characterize which subtype it is. Nowadays, the diagnosis
 258 of ATTR in the absence of a monoclonal disease can be
 259 obtained by scintigraphy with bone-seeking agent labelled
 260 with ^{99m}Tc . Instead, when a monoclonal component in
 261 serum and/or urine is present or for the diagnosis of AL, a
 262 histologic approach, often by endocardial biopsy is required
 263 [25, 26]. The major drawback of cardiac biopsy is the risk
 264 associated with the invasiveness of the technique. There-
 265 fore, researchers are trying to use non-invasive methods
 266 such as medical imaging to obtain the information needed
 267 for early diagnosis [26, 27]. In PET imaging, characteriza-
 268 tion of the CA can be performed by the evaluation of spe-
 269 cific quantitative indexes such as standardized uptake value
 270 (SUV) SUV_{\max} , SUV_{mean} and molecular volume obtained
 271 with [^{18}F]-Florbetaben by acquiring early and late static 3D
 272 images of the thorax after the injection of the radiopharma-
 273 ceutical [28–30]. Alternatively, a dynamic approach can also
 274 be taken to evaluate indexes that allow CA diagnosis [31].
 275 Being able to make an accurate differential diagnosis from
 276 a single static PET images acquired in an early phase, i.e.,
 277 after a few minutes from the injection of the tracer, should
 278 have the double advantage of reducing the waiting time for
 279
 280

281 the examination to be performed (for the patient) and obtain-
 282 ing a better organization for the nuclear medicine laboratory.
 283 Accordingly, in the present work, a set of cardiac amyloi-
 284 dosis images, consisting of 3D static PET acquired 15 min
 285 after the injection of the [18F]-Florbetaben, was used to test
 286 the goodness of the proposed approach.

287 Subjects and Cardiac PET Data Acquisition

288 A total of 47 subjects are included in this retrospective
 289 study, including 28 patients with systemic amyloidosis and
 290 heart involvement (13 patients with AL and 15 patients
 291 with ATTR cardiac amyloidosis, respectively) and 19 con-
 292 trol patients with the clinical suspicion of CA, that received
 293 an alternative diagnosis, such as left-ventricle hypertrophy
 294 secondary to aortic-valve stenosis, primary hypertrophic car-
 295 diomyopathy, or hypertensive cardiac hypertrophy. Patients
 296 with ischemic heart disease, chronic liver disease, or severe
 297 renal failure were not included in the study. Diagnosis of CA
 298 was based on clinical examination, biomarkers positivity,
 299 electrocardiogram, echocardiography, bone-scintigraphy,
 300 cardiac magnetic resonance (CMR), and histological evi-
 301 dence of amyloid deposition according to the most recent
 302 cardiological evidence and guidelines [32, 33]. Further
 303 details on patients' characteristics are described in [10]. The
 304 study was approved by the institutional ethics committee
 305 and the AIFA (Agenzia Italiana del Farmaco) committee;
 306 all subjects signed an informed consent form. The study

307 complied with the Declaration of Helsinki. Each subject
 308 underwent PET/CT examination. A Discovery RX VCT
 309 64-slice tomography (GE Healthcare, Milwaukee, WI, USA)
 310 was used for image acquisition. Firstly, a low-dose-computed
 311 tomography (CT) (tube current 30 mA, tube voltage 120 kV,
 312 effective dose of 1 mSv), covering the heart, was performed
 313 for attenuation correction. Then, 40 min of PET data were
 314 acquired, starting at the time of injection of an intravenous
 315 bolus of [18F]-Florbetaben (300 Mbq/1 ml) followed by
 316 a saline flush of 10 ml (1 ml/s). The raw PET list mode
 317 data file was histogrammed between 15 and 20 min of post-
 318 injection, to create a single static sinogram. Then, 3D static
 319 PET images were reconstructed using the ordered subset
 320 expectation maximization (OSEM) iterative algorithm with
 321 three iterations and 21 subsets. Each 3D volume consisted
 322 of 47 axial slices with a 128×128 pixels matrix.

Image Pre-processing

323 From the reconstructed axial slices of each volume, only
 324 those covering the heart were taken into consideration in the
 325 study; accordingly, for each patient, the number of images
 326 considered varied from a minimum of eight to a maximum
 327 of 19 slices. In addition, image cropping was performed.
 328 The final dimensions of the images are of 77×104 pixels.
 329 A total of 592 2D images (193 from controls, 240 from AL-
 330 subtype patients, and 159 from ATTR-subtype) have been
 331 considered in the study. In Fig. 3, examples of reconstructed
 332

Fig. 3 Example of images from the different classes: values are in SUV

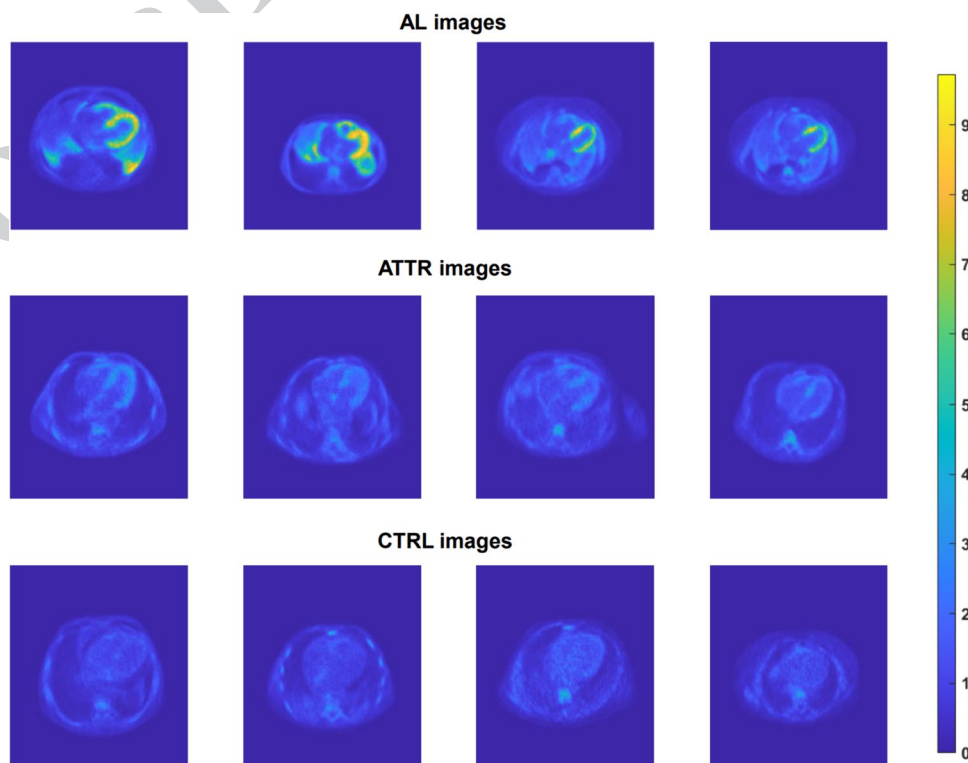
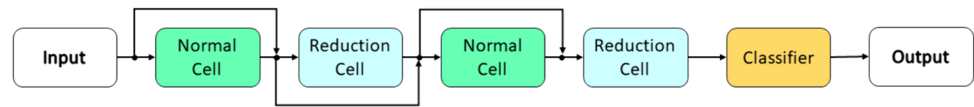


Fig. 4 Structure of the architecture we are looking for



333 and cropped images from AL, ATTR, and CTRL subjects
 334 are shown. To achieve better performance during training
 335 and avoid overfitting, data augmentation has been imple-
 336 mented. Following, an affine transformation was used [10],
 337 being recognized in literature as the most suitable method-
 338 ology for the augmentation of data sets in medical imaging
 339 [34]. Specifically, each image was randomly translated in
 340 both row and column directions of a maximum of 10 pixels
 341 and randomly rotated of maximum $\pm 10^\circ$. The affine trans-
 342 formation was applied ten times for each input image. The
 343 data augmentation is performed as a one-time preprocess-
 344 ing step and only on the training set. To avoid data leakage
 345 when evaluating the results, data splitting was performed at
 346 the patient's level, avoiding the presence of slices from the
 347 same subjects both in the training/validation and the test set.
 348 After data augmentation, the overall dimensions of the sets
 349 are the following:

- 350 • The training set consists of 384 images augmented to
 351 3840 (10× data augmentation; 1550 AL, 1010 ATTR,
 352 1280 CTRL).
- 353 • The validation set consists of 96 images (40 AL; 30
 354 ATTR; 26 CTRL).
- 355 • The test set consists of 112 images (45 AL; 33 ATTR; 34
 356 CTRL).

Hardware and Software Specs

357
 358 The overall algorithm is run on a PC, with Ubuntu Opera-
 359 tive System 22.04.3 LTS, equipped with a Core i7 4790k
 360 4-core CPU, 32GB of Ram and an Nvidia Titan Xp GPU
 361 with 12 GB of VRAM. The algorithm is implemented in
 362 Python 3.9.13 using the Anaconda environment 22.9.0 with
 363 the respective libraries. Pytorch 1.13.1 with CUDA 11.7 and
 364 CuDNN 8.5 was used for the core DL development.

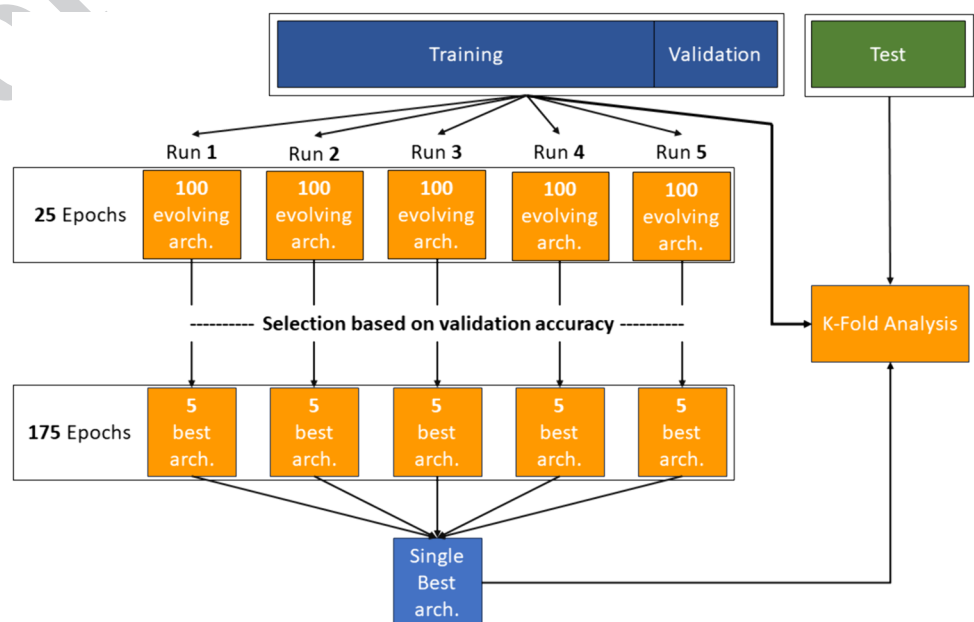
Implementation of the Algorithm and Methods Detail

365
 366 The approach used to classify the datasets is based on the
 367 method described in “Theory”.
 368

Choice of the Primitive Operations

369
 370 The primitive operations that can be used to build a normal
 371 or a reduction cell have been selected based on [9] and [19].
 372 To avoid redundancy, convolutions, max pooling, and mean
 373 pooling were restricted to 3×3 ; indeed, [9] shows that larger
 374 kernel sizes like 5×5 and 7×7 can be substituted by stacking
 375 appropriate 3×3 convolutions. In this way, each operation
 376 possesses distinct properties that cannot be substituted by
 377 others. The chosen operations are defined through a diction-
 378 ary. Following [12], 1×1 convolutions are inserted to ensure

Fig. 5 Overall performance estimation strategy and model selection



379 equal dimensions of the two hidden input states. Each convo-
 380 lution consists of a sequence of Conv-ReLU-batch normaliza-
 381 tion. Batch normalization is a popular technique used in
 382 neural networks to improve performance and stability. This is
 383 achieved by normalizing the output of a layer to have a mean
 384 of zero and a standard deviation of one [35]. This allows the
 385 network to learn more efficiently and prevents overfitting.

386 Implementation of the Evolutionary Algorithm

387 To determine the best model for the provided datasets, some
 388 parameters were set.

- 389 • The number of filters of the first cell (F) (this number is
 390 doubled before each reduction cell) was initially set equal
 391 to 4.
- 392 • The number of operations for each cell. For example, n
 393 operations correspond to $n-1$ hidden states: 2 as inputs,
 394 one as output, and the remaining $n-4$ are generated
 395 by applying the selected operations to the previously
 396 selected hidden states. The number of operations was
 397 set to 6.
- 398 • The number of classes for the classification task: equal
 399 to 3 corresponding to CTRL class (i.e., control subjects),
 400 AL and ATTR classes.
- 401 • The number of input channels is equal to one since the
 402 PET images are grayscale.
- 403 • The number of layers of the architecture is 4, as shown
 404 in Fig. 4.
- 405 • The number of starting architectures P is 100, with 900
 406 evolutionary steps C (in each step 1 sample was mutated
 407 (S)).

Table 1 Hyperparameters for the architecture search algorithm

Hyperparameter	Value
Starting number of filters F	4
Per cell operations	6
Number of classes	3
Number of channels	1
Number of layers	4
Number of starting architectures P	100
Number of evolutionary steps C	900
Number of mutated samples per step S	1
Number of training epochs	25
Number of further training epochs	175
Batch size	32
Loss function	Cross-entropy loss
Learning rate	1e-3
Optimizer	Adam (default parameters)

An example for the first convolutional operation in the
 normal cell could be:

$\mathbf{x} = \text{Conv2D}(\text{input_tensor}, F=4, \text{kernel_size}=(3, 3),$
 $\text{strides}=(1, 1), \text{padding}='same')$

$\mathbf{x} = \text{ReLU}(\mathbf{x})$

$\mathbf{x} = \text{BatchNormalization}(\mathbf{x})$

The NAS algorithm was run five times (Fig. 5). For each
 run, a first training step using 25 epochs was performed on
 a population of 100 evolving individuals, maximizing the
 overall classification accuracy. In the second step, the best
 five architectures underwent a further 175 epochs training.
 Hence, $5 \times (P + C) = 5000$ individuals were generated in
 the first step and 25 (5×5) were more deeply analyzed in
 the second step. In the final step, the best individual (i.e.,
 the one with the higher overall accuracy) was identified.
 Once the best model is selected, a stochastic k -fold vali-
 dation of the best model is performed using five random
 splits of the training/validation dataset. All the training
 was done using the Adam optimizer, with a learning rate

Table 2 Best five individuals for each of the five runs

Individual #	Initial validation accuracy (25 epochs)	Final validation accuracy (175 further epochs)
1st RUN	5	75.00%
	250	65.63%
	421	63.54%
	688	63.54%
	990	78.13%
2nd RUN	363	76.04%
	376	68.75%
	849	80.21%
	878	85.42%
	887	81.25%
3rd RUN	372	85.42%
	487	66.66%
	562	76.04%
	666	65.63%
	995	82.29%
4th RUN	49	69.79%
	129	71.88%
	268	72.91%
	342	65.63%
	929	73.96%
5th RUN	8	59.38%
	472	73.96%
	602	70.83%
	669	77.08%
	799	77.08%

427 of $1e-3$, cross-entropy loss, and a batch size of 32. Detailed
 428 values of the hyperparameters used for the architecture
 429 search algorithm are shown in Table 1.

Pseudocode for the implemented algorithm is provided
 below. From top to bottom, changing color: initialization,
 initial population setup, evolutionary algorithm, final
 training of the best architectures and output.

430
 431
 432
 433

```

population = queue[]
history = array[]
top5_models = array[]
P = 100
C = 900
num_classes = 3
input_channels = 1
layers = 4
mutations = [identity, hidden_state_mutation, operation_mutation]
probabilities = [0.05, 0.475, 0.475]

while length(population) < P:

    model.instantiate(ModelClass)
    model.define_random_architecture(num_classes, input_channels, layers)
    model.train_and_evaluate(epochs = 25)
    population.push(model)
    history.add(model)

while length(history) < P + C:

    parent = history.sample()
    child.instantiate(ModelClass)
    child.architecture <- parent.architecture
    child.random_mutate(mutations, probabilities)
    child.train_and_evaluate()
    population.push(child)
    population.pop()
    history.add(child)

history.select_top5_accuracy()

for model in history:

    model.train_and_evaluate(epochs = 175)
    top5_models.add(model)

return history, top5_models
  
```

434 **CAclassNET as Handcrafted Neural Network** 435 **for Comparison**

436 To evaluate the goodness of the net obtained by the NAS
 437 methodology, a comparison was made with the CNN, named

CAclassNET, previously proposed by the authors in [10]. In
 the present work, the CAclassNET was newly implemented
 by using Python and Pytorch facilities (in [10], it was imple-
 mented in Matlab), for a better comparison between the two
 networks, and trained with the optimized hyperparameters

438
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443 described in [10]. The training was then repeated five times
 444 to statistically evaluate the performance of the classifier on
 445 the provided dataset.

446 Results

447 The initial and final validation accuracy results for each
 448 individual architecture among the best five are reported in
 449 Table 2 for each run.

450 Accuracy values were normally distributed ($p=0.485$,
 451 Shapiro-Wilkinson test). One-way analysis of variance
 452 (ANOVA) detected no significant accuracy difference
 453 ($p=0.829$) in the five final validation runs (Table 2). Tukey
 454 test has been used to detect anomalous observations in accu-
 455 racy values, and no outliers have been detected. Of the five
 456 runs, the second run yielded the best validation accuracy,
 457 achieved by individual 363, with a final accuracy of 90.63%.
 458 The relevant confusion matrix for the validation set is shown
 459 in Fig. 6. According to such results, further deep analysis
 460 was performed on this net (NAS-Net in the following).

461 The structure of the normal and reduction cells is shown
 462 in Fig. 7; the first two hidden states, c_{k-2} and c_{k-1} , represent
 463 the two inputs of each cell, while c_k represents the output
 464 state.

465 As shown in Fig. 7, two kinds of convolution are used:
 466 dilated convolutions (DIL_CONV) and dilated separable
 467 convolutions (SEP_CONV). Each convolution operation
 468 consists of a sequence: 1. convolution; 2. ReLU; 3. batch
 469 normalization (BN). For separable convolutions, these oper-
 470 ations are repeated twice [12]. The NAS-Net was trained five
 471 times, splitting the training and validation entries differently

472 in a stochastic manner to statistically evaluate the perfor-
 473 mance of the classifier. For each run, the parameters were
 474 reset.

475 Figure 8 shows the validation and training loss of the
 476 classifier over epochs; continuous lines are the mean values
 477 of the five runs, and shadowed regions cover 95% of the
 478 confidence interval. For each run, the performance of the
 479 NAS-Net on the test set (unseen data) was also evaluated.

480 Figure 9 shows two examples of confusion matrices
 481 obtained during the different runs (the best and the worst
 482 runs, respectively). Table 3 summarizes the overall classifier
 483 performances, evaluated in terms of sensitivity, specificity,
 484 and accuracy. From repeated measurements ANOVA analy-
 485 sis, it results that sensitivity and specificity values in all three
 486 comparisons (i.e., AL vs. ATTR, AL vs. CTRL, and ATTR
 487 vs. CTRL) as well as accuracy values in AL vs. ATTR and
 488 AL vs. CTRL, are significantly different ($p < 0.001$); no sig-
 489 nificant difference was detected between ATTR vs. CTRL
 490 accuracy values ($p = 0.173$). The overall mean accuracy of
 491 the best classifier for the test set was 76.95% ($\pm 2.13\%$). The
 492 time needed for a single run of the evolutionary algorithm
 493 and to evaluate the 5 best architectures was, on average,
 494 about 12 h and 30 min. Every subsequent retraining of the
 495 best model required about 20 min.

496 Comparison with the Handcrafted Neural Network

497 The average accuracy of the CAclassNET was 99.38% for
 498 the training set and 87.35% for the validation set. Table 4
 499 shows the performance of the handcrafted classifier as meas-
 500 ured by sensitivity, accuracy, and specificity. Similarly to
 501 the results of Table 3, also for Table 4, the ANOVA analysis
 502 was performed: sensitivity and specificity values in all three
 503 comparisons, as well as for accuracy values in AL vs. ATTR
 504 and AL vs. CTRL, are significantly different ($p < 0.001$);
 505 no significant difference was detected between ATTR vs.
 506 CTRL accuracy values ($p = 0.8$). The overall accuracy on
 507 the test set was 79.21% $\pm 3.4\%$. The performances in terms
 508 of sensitivity, accuracy, and specificity are better than those
 509 of a doctor with more than 10 years of experience in cardiac
 510 nuclear medicine in fact, they resulted to be as follows [10]:
 511 sensitivity, specificity, and accuracy equal to 0.533, 0.744,
 512 and 0.673 respectively for AL patients, 0.314, 0.802, and
 513 0.665 for ATTR patients, 0.562, 0.667, and 0.627 for CTRL.

514 Table 5 summarizes the differences between the two mod-
 515 els in four aspects: number of parameters, time to define
 516 an architecture, training time, and classification time of a
 517 new image. Regarding accuracy at the subject level, both
 518 the architecture developed using the NAS method and
 519 CAclassNET are able to consistently and correctly identify
 520 8 (3 CTRLs, 3 ALs, 2 ATTRs) out of the 11 (5 CTRLs, 3
 521 ALs, 3 ATTRs) subjects in the test dataset. Note that ALs
 522 are always correctly classified.

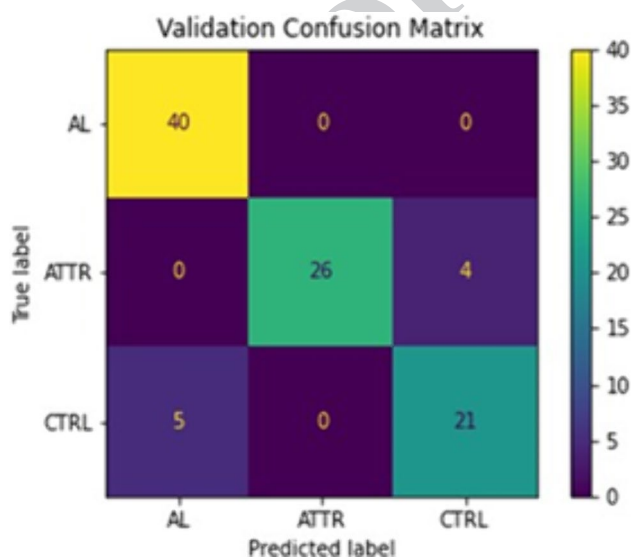


Fig. 6 Confusion matrix on the validation set for the best model

Fig. 7 Graphs describing the architecture of the normal (top) and reduction (bottom) cell

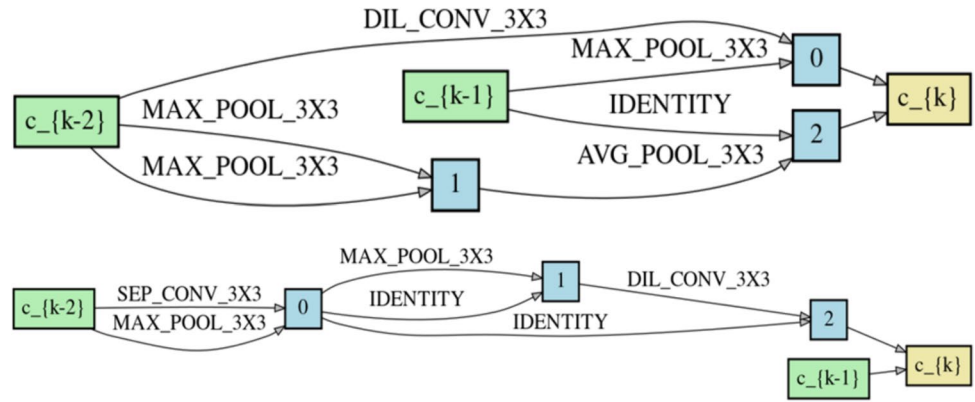
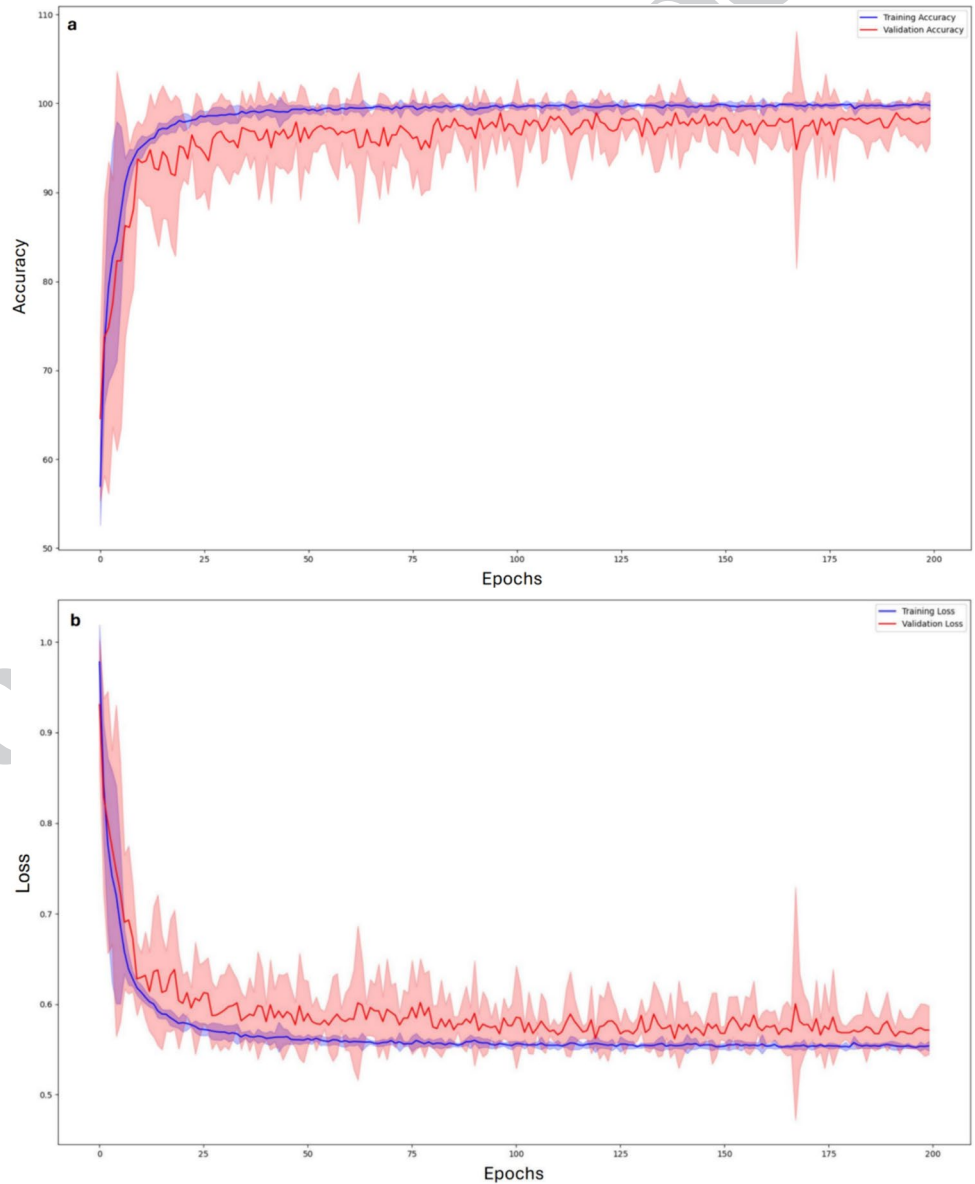


Fig. 8 Average training (blue) and validation (red) accuracy (a) and loss (b) with 95% confidence intervals (shaded areas). On the x-axis the epochs



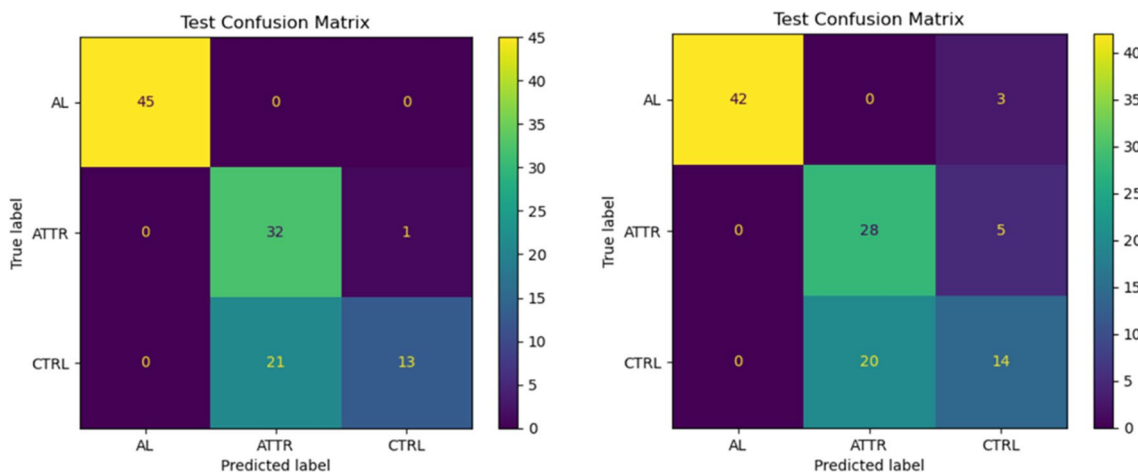


Fig. 9 Best (left) and worst (right) confusion matrices obtained during two of the five runs

Table 3 Performance of the NAS-Net model (%)

Class	Sensitivity	Accuracy	Specificity
AL	98.7 ± 2.9	99.3 ± 1.1	99.7 ± 0.7
ATTR	93.3 ± 7.8	78.0 ± 2.9	70.9 ± 3.7
CTRL	35.8 ± 14.6	77.1 ± 2.0	96.7 ± 4.4

Table 4 Performance of the CAclassNET classifier (%)

Class	Sensitivity	Accuracy	Specificity
AL	99.0 ± 1.6	99.6 ± 0.6	100.0 ± 0.0
ATTR	76.2 ± 14.0	79.6 ± 3.5	80.1 ± 5.6
CTRL	55.8 ± 11.0	79.2 ± 3.3	89.4 ± 6.2

AQ8 Table 5 Comparison between the best architecture discovered by the NAS algorithm (NAS-Net) and CAclassNET

Features	NAS-Net	CAclassNet
Number of parameters	2.763 × 10 ³	93.827 × 10 ³
Implementation time	~8 h per 1000 architectures evaluated	days/weeks
Training time (200 epochs) [s]	224.67 (≈ 3'45'')	187.06 (≈ 3'7'')
Classification time of a new image [ms]	6.4	3.4

523 Discussion

524 Contribution of This Work

525 The main objective of this study was to demonstrate
 526 the effectiveness of the neural architecture search algorithms for medical image classification, early acquired
 527

[18F]-Florbetaben PET images in particular. The use of NAS methods for defining the best model for image analysis has the great advantage of greatly reducing the operator's contribution in defining the structure and parameters to be used, making these operations almost completely automatic. Therefore, the effort required to design the deep learning models is reduced, and researchers can focus on other aspects, such as data pre-processing and model tuning, improving the performance of the models found. Unlike ordinary images, in which large databases are available online, the analysis of medical images using deep learning methods is often challenging due to privacy concerns and the rarity of certain pathologies. This is especially true for PET images, where datasets are increasingly limited. In literature, some attempts have been made, and some methods based on the NAS approach have been proposed on medical images, mainly for image segmentation [9], but, as far as we know, there are no studies on the classification of cardiac amyloidosis from early acquired [18F]-Florbetaben PET images; in fact, we can state that only the authors have implemented a CNN that performs this task [10], but not using NAS technology.

550 Methodology

551 The cell-based search space method was selected in this
 552 work. This search space consists of architectures composed of repeating blocks of two main types: normal and reduction cells. Each cell consists of a DAG that describes how the different states are combined to form a new state using primary operations. Search space is then explored using an aged evolutionary algorithm: the oldest individual in history dies at each generation. The results obtained after running the proposed NAS approach

560 five times, after 25 epochs had an accuracy from a mini-
 561 mum of 59.38% (see Table 2, fifth run) to a maximum of
 562 85.42% (see Table 2, second and third run), with a mean
 563 value of 73.04%. Therefore, already after 25 epochs, the
 564 NAS approach has given quite promising results. But the
 565 results obviously improved after a further 175 epochs,
 566 bringing the accuracy to a minimum value of 65.63% (see
 567 Table 2, fifth run) and a maximum of 90.63% (Table 2,
 568 second run) with a mean of 79.24%. The model giving the
 569 highest accuracy has been considered as the network for
 570 cardiac amyloidosis classification. The proposed two-step
 571 approach was designed to obtain a reasonable process-
 572 ing time for individual selection. The structure of the best
 573 network model obtained by the proposed NAS approach
 574 (NAS-Net) is shown in Figs. 4 and 7; the behavior of the
 575 architecture as a graph is evident both for the structure as a
 576 whole and for the individual cells. The identity operations
 577 in the reduction cell (Fig. 7) are introduced to maintain the
 578 network's depth constant.

579 Results

580 The confusion matrix obtained for the network with
 581 higher validation accuracy (see Fig. 6) demonstrates that
 582 the determination of the cardiac amyloidosis AL class is
 583 optimal, with some uncertainty between the ATTR class
 584 and controls. Training and validation accuracy trends of
 585 the selected model, shown in Fig. 8, have a typical shape in
 586 network analysis: both curves increase over epochs as the
 587 model learns to make more appropriate predictions on both
 588 sets. A gap exists between training and validation curves
 589 being training higher than validation; this is expected and
 590 mainly due to the low number of data available as it hap-
 591 pens to all imaging techniques that require, for example,
 592 the use of ionizing tracers and/or invasive maneuvers for
 593 which images are acquired only if strictly necessary. How-
 594 ever, it is worth to note that at 200 epochs the accuracy
 595 for validation data is anyway quite high, having the mean
 596 value equal to 98.3% (see Fig. 8). Also, for training and
 597 validation losses both curves decrease over epochs. This
 598 is an indication that the model is learning to make more
 599 accurate predictions for the training and validation set.
 600 Both confusion matrices (Fig. 9) and sensitivity, accuracy,
 601 and specificity values (Table 3) show that the network well
 602 determines AL cardiac amyloidosis patients. In contrast,
 603 ATTR amyloidosis patients and controls are sometimes
 604 incorrectly diagnosed, with NAS-Net privileging sensitiv-
 605 ity for ATTRs (93.3%) and specificity for CTRLs (96.7%).
 606 This is well documented in literature where it is asserted
 607 that the cardiac PET imaging using [18F]-Florbetaben well
 608 characterizes the presence of type AL amyloidosis, while
 609 it is not able to determine the ATTR and to distinguish it
 610 from other pathologies or from the non-presence of cardiac

611 pathology [30]. This is even true when considering early
 612 acquired images, i.e., at 15 min after injection [10], as it
 613 is in our study. On the other hand, by reducing the clas-
 614 sification task to AL vs. non-AL subjects, the performance
 615 of the discovered classifier is optimal, well identifying
 616 subjects affected by CA of type AL. To demonstrate the
 617 validity of the proposed approach, that is, it automatically
 618 generates an optimal network that is comparable with the
 619 best one obtainable manually, a comparison has been made
 620 with a state-of-art handcrafted CNN, carefully tuned on
 621 the same data set. In fact, from Tables 3 and 4, we can see
 622 that the two networks showed a similar performance pat-
 623 tern, with very good sensitivity, accuracy, and specificity
 624 values for the AL class and lower values for ATTR and
 625 CTRL classes. All values were >70% except for the CTRL
 626 sensitivity value for both networks. Moreover, in Table 5,
 627 the performances of the two nets are compared, showing
 628 a 40 times higher value of the number of parameters for
 629 the CAclassNet, while the training processing time and the
 630 classification time of a new image are slightly higher for
 631 NAS-based net. Overall, we can say that the NAS-based
 632 algorithm found a model whose performance is compara-
 633 ble to that available in the literature. Indeed, it correctly
 634 discriminates between AL and non-AL images but shows
 635 intermediate performance in classifying ATTR and CTRL.

Advantages, Disadvantages, and Limitations

636 The implementation of this approach made it possible to
 637 clearly highlight both the advantages and disadvantages of
 638 this technique. A great advantage is that the best architecture
 639 can be automatically identified that is better suited to the
 640 specific problem at hand. The disadvantage is the computa-
 641 tional cost since multiple neural networks must be trained
 642 and evaluated to find the best one. In this work, to reduce
 643 this weakness, we reduced the number of training epochs
 644 to speed up the process of exploring search space. Then,
 645 the best architectures were trained for more epochs to find
 646 the best-discovered model. However, it is worth noting that
 647 such optimal parameters search phase, which requires high
 648 processing times, in conventional methods has still to be
 649 performed, and it is done with the continuous contribution
 650 of the operator and, therefore, not automatically. While the
 651 definition and training of CAclassNET required repeated
 652 architecture evaluations and, only subsequently, hyperpa-
 653 rameter tuning, the evolutionary algorithm set for the NAS
 654 network automatically selects the best architecture once
 655 the hyperparameters are specified (Table 1). In the present
 656 work, these hyperparameters were set according to empiri-
 657 cal knowledge in NAS literature, reducing the time required
 658 for hyperparameter search. One hidden cost that could also
 659 be considered is the human-production cost associated with
 660

661 the implementation of the code used for this work, which,
662 however, can be reused as an asset for future model develop-
663 ment (code once, run forever).

664 The network generated here with the NAS method is
665 aimed at classifying amyloidosis from PET data; in the pre-
666 sent work, we have not evaluated whether this net can be
667 adapted to other image classification tasks. Anyway, we sup-
668 pose that, either by re-running the evolutionary algorithm on
669 new data/with different hyperparameters or with appropriate
670 network modifications typical of transfer learning, the meth-
671 ods shown in this work could be used for the development of
672 any convolutional model for the classification of biomedical
673 images (or even other tasks, with appropriate modifications).

674 One limitation in this work is the low amount of data:
675 data relevant to 47 subjects are considered, for a total of 592
676 2D PET images. This is not a lot of data for deep learning
677 analysis, as it is often the case for biomedical images. But
678 one of the purposes of this work was precisely to evaluate
679 whether the NAS methodology was efficient even when the
680 data available is rather limited.

681 Conclusions

682 In the present work, the NAS approach was applied to clas-
683 sify medical images. In particular, the main objective has
684 been to evaluate the possibility of automatically finding an
685 optimal network for the classification of cardiac amyloido-
686 sis from [18F]-Florbetaben PET images acquired 15 min
687 after injection. The results obtained are very promising,
688 being very similar to those available in the literature for
689 CNNs designed manually, while for the proposed approach
690 this task was carried out completely automatically.

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695 and design. All authors read and approved the final manuscript.

696 **Data Availability** Data used in this article are not available due to it
697 being property of the healthcare institution.

698 **Code Availability** Developed code is available upon request to the cor-
699 responding author.

700 Declarations

701 **Ethics Approval** Relating to the data used in this article, both the AIFA
702 (Agenzia Italiana del Farmaco) committee and the institutional ethics
703 committee gave their approval to the study. The research complied with
704 the Helsinki Declaration.

705 **Competing Interests** The authors declare no competing interests.

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